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# Selective Indicators for Optical Determination of Disease Biomarkers

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## Recommended Citation

Hakuna, Lovemore, "Selective Indicators for Optical Determination of Disease Biomarkers" (2014). Dissertations and Theses. Paper 2053. <https://doi.org/10.15760/etd.2052>

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Selective Indicators for Optical Determination of Disease Biomarkers

by

Lovemore Hakuna

A dissertation submitted in partial fulfillment of the requirements for the degree of

> Doctor of Philosophy in **Chemistry**

Dissertation Committee: Robert M. Strongin, Chair Carl C. Wamser Reuben H. Simoyi Jonathan Abramson

Portland State University 2014

## **ABSTRACT**

The most abundant biological thiols, homocysteine (Hcy), cysteine (Cys) and glutathione (GSH) have been the subject of intense research due to their association with a wide range of diseases. They play a key role in maintaining the redox status of biological systems. Selective detection methods for these thiols are challenging due to their similar structures and properties. Current commercially available detection methods use separations, fragile and expensive enzymatic or immunogenic materials and complex instrumentation. This has led to a global effort towards developing simple and inexpensive optical probes and indicators selective for specific biological thiols.

Highly selective chemical probes and simple methods for detection and potential quantification of Hcy and GSH in their natural biological media have been developed. These indicators and methods are relatively simple and inexpensive for potential application at point of care. The selective detection of Hcy using novel asymmetric viologen chemical probes at room temperature is described as well as the use of commercially available materials under photochemical conditions. These probes respond linearly proportional to increasing Hcy concentrations, potentially enabling the monitoring of Hcy levels in human plasma. Additionally, new methods for the selective determination of GSH in human plasma, as well as its quantitation in whole blood deposited on filter paper (dried blood spots), is also presented herein.

## **DEDICATION**

*In the fullness of time God makes all things possible. Thank you Lord, thus far you have taken me!*

*To my beloved mother, it has been 8 years since you departed but it feels like yesterday, I love you and thanks for all your sacrifices.*

#### **ACKNOWLEDGEMENTS**

Firstly, I would like to express my sincere gratitude to my research advisor,

Dr Robert M. Strongin for his invaluable support, professional guidance and affording me the opportunity to work in his group.

My special thanks are extended to my research committee members, Dr. Carl C. Wamser, Dr. Reuben H. Simoyi and Dr Jonathan Abramson for their time and support in my studies.

To Dr. Jorge Escobedo, Dr. Martha Sibrian-Vazquez and Dr Mark Lowry, thanks for all your expertise and massive knowledge you shared with me during the course of my studies. I wish to acknowledge my former and current colleagues, Brandon Doughan for assisting with method optimization, Dr Soojin Lim, Aabha Barve, Yixing Guo, Davin Rautiola, Thomas Seidl, Jialu Wang, Shelly Chu, Lei Wang for their support. I'm also very grateful for the assistance provided by Dr. Wilbes Mbiya with EPR studies and Nicholas Day with cyclic voltammetry work.

Finally, I would like to express my deepest gratitude to my family for their prayers, moral support and encouragement throughout my studies especially the love of my life, Nolline and my beloved son, Sean Tinotenda. Thank you for your love and sacrifices to make this dream come true.

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### **CHAPTER 1: INTRODUCTION**

#### **1.1 Background and significance of homocysteine (Hcy)**

1.1.1 Structures and composition of biological thiols

Biothiols such as homocysteine (Hcy), glutathione (GSH) and cysteine (Cys), (structures shown in Figure 1.1) play significant roles in regulating various biological processes. GSH, a tripeptide γ-glutamyl-cysteinyl-glycine is the major non-protein intracellular thiol which apart from being an important antioxidant, also regulates cellular functions such as gene expression, cell proliferation and apoptosis.<sup>[1-3](#page-107-0)</sup> GSH concentrations in cells range from 1–10 mM whereas plasma levels range from 1–6  $\mu$ M.<sup>[1](#page-107-0)[,4-7](#page-107-1)</sup> Cys is the most abundant low-molecular-weight thiol in plasma and plays a fundamental role in protein synthesis, cell metabolism and detoxification.<sup>[8](#page-107-2)</sup> It is a precursor of GSH and its structure closely resembles that of Hcy. Healthy levels of Cys range from 135–300 μM and its abnormal levels are associated with various disease states such as liver damage, edema and skin lesions.<sup>[7,](#page-107-3)[9-11](#page-108-0)</sup>

Hcy is a metabolic intermediate derived from the essential amino acid methionine in the biosynthesis of  $Cys$ <sup>[12](#page-108-1)</sup> Structurally, Hcy differ from  $Cys$  by a single methylene group (Figure 1.1) which makes their individual determination very challenging. It exists in various forms in plasma with the most dominant one being the protein bound accounting for 70-80% of total Hcy, followed by the free oxidized form (non-proteinbound disulfides) constituting 20% and finally free, reduced Hcy making up less than

1% of the total pool.<sup>[7](#page-107-3)</sup> Plasma total homocysteine (tHcy) refers to the sum of all the three forms (all circulating disulfides and reduced Hcy).

Normal plasma tHcy concentrations range from 5–15 μM. At elevated levels, a condition known as hyperhomocysteinemia occurs that is an independent risk factor for several major pathologies such as cardiovascular disease (CVD), dementia, osteoporosis and Alzheimer's disease.<sup>[13-15](#page-108-2)</sup> Hyperhomocysteinemia is classified into three categories including moderate (15–30  $\mu$ M), intermediate (30–100  $\mu$ M) and severe (>100  $\mu$ M).<sup>[7](#page-107-3)[,16](#page-109-0)</sup> Due to the relationship between hyperhomocysteinemia and lower methionine synthase activity and folate deficiency, it has been proposed that folate therapy may be useful for for hyperhomocysteinemia-related disorders.<sup>[17](#page-109-1)</sup>



Figure 1.1. Structures of selected biological thiols.

#### 1.1.2 Significance of Hcy to public health

Hcy plays a critical role in methionine and folate metabolism. It is a metabolic intermediate that participates in two pathways, the re-methylation (methionine cycle) and transsulfuration (folate cycle, Figure 1.2).<sup>[18](#page-109-2)[,19](#page-109-3)</sup> In the re-methylation pathway, Hcy receives a methyl group from 5-methyltetrahydrofolate (most common in cells and tissues) or betaine and is reconverted to methionine, which is fundamental to biochemical processes such as protein and nucleic acid synthesis. In the transsulfuration pathway, Hcy is converted to Cys through cystathionine in a reaction involving serine and catalyzed by a vitamin B6 dependent enzyme, cystathionine-β-synthase. This pathway is irreversible indicating the inability of Cys to serve as a precursor for methionine. Most Cys formed is in turn converted to the tripeptide GSH.



Figure 1.2. Pathways for the metabolism of Hcy.<sup>[18,](#page-109-2)[19](#page-109-3)</sup>

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Elevated plasma levels of Hcy  $^{20,21}$  $^{20,21}$  $^{20,21}$  $^{20,21}$  can be caused by metabolic defects in the two pathways or deficiencies of enzymes and cofactors required in these pathways. Hyperhomocysteinemia can be caused by the impaired synthesis of 5 methyltetrahydrofolate due to the deficiency of folate or a defect in methylenetetrahydrofolate reductase (MTHFR).<sup>[12](#page-108-1)</sup> In these cases, Hcy meant for remethylation would be channeled to the transsulfuration pathway thereby decreasing the intracellular s-adenosylmethionine (SAM) concentration as well as overburdening the transsulfuration system with excess Hcy. The additional Hcy coupled with lower concentrations of SAM (not sufficient to activate cystathionine synthesis) damage the transsulfuration pathway. Eventually, Hcy accumulates in cells and is consequently exported into the blood causing hyperhomocysteinemia.<sup>[12,](#page-108-1)[19,](#page-109-3)[22](#page-109-6)</sup>

4 Another cause of hyperhomocysteinemia is a defect in cystathionine-β-synthase that impairs the transsulfuration pathway via the diversion of Hcy towards the remethylation pathway. This increases the rate at which methionine is synthesized leading to a rise in the level of intracellular SAM. The level of SAM can reach a point where it causes feedback inhibition of MTHFR, thus blocking the re-methylation process. This leads to severe hyperhomocysteinemia because both pathways would have been impaired.<sup>[12,](#page-108-1)[22](#page-109-6)</sup> Abnormalities in the enzyme cystathionine-β-synthase also cause homocystinuria which is an autosomal recessive disorder characterized by ocular lens dislocation, mental retardation and aggressive vascular disease, in particular venous thromboembolism.[18](#page-109-2) Other factors which have been reported to cause hyperhomocysteinemia include environmental toxins as well as poor nutrition and lifestyle. For example, cigarette smoking, a high intake of alcohol and caffeine are associated with increased Hcy levels.<sup>[23](#page-110-0)</sup> Hcy concentrations rise in diseases such as cancer, hypothyroidism, inflammatory bowel and end-stage renal disease.<sup>[20,](#page-109-4)[24,](#page-110-1)[25](#page-110-2)</sup> Hcv levels rise with age, and women generally have lower levels than men but the concentrations rise after menopause.<sup>[26,](#page-110-3)[27](#page-110-4)</sup>

Several studies have been published showing an association between elevated levels of Hcy and CVD. A strong link between plasma Hcy and CVD mortality has been established in an early study by the World Health Organization (WHO). [28](#page-110-5) Nygard, *et al*., in their 2001 study, discovered that the cardiovascular related mortality ratios doubled when Hcy levels were twice as high. $29$  Meta-analyses of both prospective and genetic studies demonstrated that there is a significant association between Hcy levels and CVD. In these studies it was predicted that lowering tHcy by 3 µmol/L (by increasing folic acid intake) would reduce the risk of heart disease by  $11-16\%$ , thrombosis by 25% and stroke by 19–24%. [30](#page-111-0)[,31](#page-111-1) A recent study by Bertoia, *et al*., found that higher Hcy levels were positively associated with a risk of peripheral artery disease in men.<sup>[32](#page-111-2)</sup> It has been reported that each 5 µmol/L increase in Hcy level increases the risk of coronary heart disease (CHD) events by approximately 20%, independently from traditional CHD risk factors. In the Multi-Ethnic Study of Atherosclerosis (MESA), it was found that higher Hcy levels were significantly associated with a higher incidence of CVD and CHD.<sup>[33](#page-111-3)</sup>

Meta-analysis genetic studies have also given further evidence showing the casual relationship between elevated tHcy and CVD. The homozygous mutant for MTHFR C677T polymorphism which affects about 10% of individuals worldwide results in

impaired folate metabolism and elevated tHcy levels.<sup>[34](#page-111-4)</sup> Three meta-analyses involving over 25,000 cases examined the impact of this genetic variant (homozygous MTHFR polymorphism) on heart disease risk and found that the risk was higher in individuals with polymorphism compared to those without the polymorphism by about  $14{\text -}21\%$ .<sup>[30,](#page-111-0)[35](#page-111-5)[36](#page-111-6)</sup>

In another study, the relationship between MTHFR polymorphism and the severity of coronary artery disease in patients undergoing coronary artery bypass surgery showed that Hcy levels were significantly higher in patients with coronary artery disease than in control subjects. $37$ 

Hcy has also been associated with neural tube defects, increased incidence of dementia, inflammatory bowel disease and osteoporosis.<sup>[38](#page-112-1)[,39](#page-112-2)</sup> In addition, elevated Hcy can be used to diagnose and follow the progression of cardiovascular disease in cases where classical risk factors such as hypertension, diabetes and hyperlipidemia are absent. Therefore a compelling case can be made for detecting and treating hyperhomocysteinemia in patients with a history of premature cardiovascular disease, stroke, or venous thromboembolism.[40](#page-112-3)

### **1.2 Hcy controversy**

Although significant research has shown that Hcy is a risk factor at even modestly elevated levels,<sup>[41](#page-112-4)</sup> the role of Hcy in cardiovascular diseases is not clear and has been debated for decades as to whether it is just a biomarker or actually a risk factor. However, according to the 2006 government study published in *Circulation* by Yang, Q., *et al.*,

strong evidence was provided showing the association between Hcy and cardiovascular risk.<sup>[42](#page-112-5)</sup> They found that folate fortification (for lowering Hcy levels) significantly reduced deaths from strokes and heart attacks. More recent studies confirmed that homocysteine is a strong, independent CVD predictor. [43](#page-112-6) More so, Wang *et al.*, in their meta-analysis on the efficacy of folic acid supplementation in stroke prevention concluded that folic acid supplementation can effectively prevent stroke in populations with no or partial folic acid fortification.[44](#page-113-0)

On the other hand, a meta-analysis of the Cochrane Database of Systematic Reviews published by Carvajal *et al*., 2009 indicated that Hcy lowering therapy did not reduce the risk of myocardial infarction and stroke.<sup>[45](#page-113-1)</sup> In another recent study, it was concluded that folic acid based homocysteine lowering does not reduce cardiovascular events in people with kidney disease.<sup>[46](#page-113-2)</sup> Numerous secondary intervention trials involving lowering Hcy levels by vitamin supplementation have been performed recently but none afforded conclusive evidence of generally improved CVD outcomes.<sup>[47](#page-113-3)[,48](#page-113-4)[49](#page-113-5)[,50](#page-113-6)</sup> However, it should not be assumed that no relationship exists because such studies conflict with a massive body of published evidence clearly showing that Hcy is toxic at even modestly elevated levels.<sup>[47](#page-113-3)[,51](#page-114-0)</sup> They contradict other clinical trials (e.g., the NIHLB's Framingham study) in the broader CVD biomarker field that view Hcy monitoring as useful, for instance, in clinical situations wherein CVD patients are asymptomatic and/or traditional risk factors are not elevated or had been already well-controlled.<sup>[52](#page-114-1)</sup>

Several explanations for the intriguing and conflicting clinical trial outcomes have been reported and these include:  $47,53$  $47,53$ 

- (i) homocysteine-lowering trials could have been underpowered by the duration of follow-up which has been too short as shown in the meta-analysis of the effect of B vitamins on stroke.<sup>[54](#page-114-3)</sup> The result of this study was a full absence of any effect in the short-term but a statistically significant 29% reduction in the studies with at least 36 months of follow-up;
- (ii) vitamin supplements given to lower Hcy levels have themselves been shown to exacerbate CVD, and therefore negated any benefits of Hcy lowering;
- (iii) cohorts recruited all had advanced atherosclerotic disease and thus Hcy had apparently already done its major damage in mediating progression, rendering lowering Hcy interventions too late;
- (iv) since elevated Hcy levels can arise from and impact a highly complex set of pathogenic mechanisms, more specifically targeted mechanism- and/or patient-specific interventions than relatively simple vitamin supplementation may be needed to effectively manage CVD via targeting Hcy levels;
- (v) interpretation of the results from these large vitamin trials may have been incorrect due to statin/aspirin therapy, which was applied along with the vitamin and folic acid fortification.

Despite this controversy, the consistency in published evidence showing a strong relation between hyperhomosysteinemia and cardiovascular related diseases renders Hcy determination of clinical significance.<sup>[47](#page-113-3)</sup>

## **CHAPTER 2: HCY DETECTION METHODS**

## **2.1 Current clinical methods**

The clinical relevance of Hcy as a diagnostic risk factor for CVD has justified the need to develop rapid, precise, and accurate techniques for detecting and quantifying tHcy. Currently, there are three main tHcy testing methods that are used in clinical laboratories including chromatographic (analytical HPLC with a derivatization step, gas chromatography/mass spectrometry (GC-MS)), immunoassays and enzymatic assays. [38](#page-112-1)[,41](#page-112-4)[,55](#page-114-4)[,56](#page-114-5) While the HPLC method has high precision and sensitivity, it often requires skilled staff, is labor intensive and throughput may be low.<sup>[38,](#page-112-1)[57](#page-114-6)</sup> The need for derivatization introduces additional sample processing steps hence it's not the method of choice in major clinical laboratories. GC-MS uses complex instrumentation that is not typically applied at point-of-care and requires tedious procedures not suitable for routine diagnostic applications.

10 Immunoassays and enzymatic methods use antibodies and biomolecules that are relatively expensive and fragile; therefore, careful attention to storage conditions is required.[58](#page-115-0) Despite those shortcomings, the enzyme cycling assay is becoming the preferred method for clinical laboratories involved in routine screening applications over the immunoassays and chromatographic approaches because it uses less reagents, does not require sample pre-treatment and offers high throughput.<sup>[58,](#page-115-0)[59](#page-115-1)</sup> Hcy assay interference from hemolysis, icterus, and lipemia has been reported with the hemoglobin interference being the most prevalent.<sup>[60](#page-115-2)</sup> Large differences between the methods used and the different

testing laboratories have been reported creating the need for more standardization of tHcy testing methods.<sup>[55,](#page-114-4)[61,](#page-115-3)[62](#page-115-4)</sup>

## **2.2 Optical methods**

Optical techniques including colorimetric or fluorescence and luminescent have received increased attention over other analytical methods because they offer a number of advantages such as operational simplicity, low cost, suitability for monitoring intracellular analytes and high sensitivity.<sup>[63,](#page-115-5)[64](#page-115-6)</sup> A wide variety of useful optical detection probes for biological thiols based on different mechanisms has been reported.<sup>[65-67](#page-116-0)</sup> Most have no specificity for Hcy over other structurally related analytes such as Cys and GSH. Selective determination of plasma tHcy levels (normal,  $5-15 \mu M$ ) is further complicated by the higher levels of Cys (135–300  $\mu$ M) almost 20 times that of Hcy and comparable levels of GSH  $(1–6 \text{ uM})$  $(1–6 \text{ uM})$  $(1–6 \text{ uM})$ .<sup>6[,7](#page-107-3)[,10](#page-108-3)[,16](#page-109-0)</sup>

#### 2.2.1 Hcy/Cys selective probes over GSH

Most probes can distinguish Cys/Hcy from GSH and recent examples include a commercially available chromophore, 4-chloro-7-nitro-2,1,3-benzoxadiazole (NBD-Cl) reported by Niu and co-workers (Figure 2.1).<sup>[68](#page-116-1)</sup> The proposed mechanism involves intramolecular displacement of chloride by thiolate followed by replacement of the thiolate with the amino groups of Cys/Hcy, but not GSH to form amino-substituted products which show strong fluorescence compared to that exhibited by the sulfursubstituted product for GSH.



Figure 2.1. Substitution reaction of NBD-Cl (4) with aminothiols.<sup>[68](#page-116-1)</sup>

Goswami *et al*., developed a turn on excited-state intramolecular proton transfer (ESIPT) probe, 5(benzothiazol-2-yl)-4-hydroxyisophthalaldehyde (BHI) for rapid and ratiometric fluorogenic detection of Hcy and Cys over other amino acids (Figure 2.2).<sup>[69](#page-116-2)</sup> This probe, however cannot discriminate between Hcy and Cys.



Figure 2.2. Reaction of **7** with Hcy/Cys. [69](#page-116-2)

## 2.2.2 Hcy selective probes

Though some chemosensors or chemodosimeters that selectively respond to Hcy over Cys and other thiols have been reported, they are typically tested at equimolar, rather than more natural *ca*. 20-fold excess Cys concentrations.<sup>[70-72](#page-116-3)</sup> A phosphorescent sensor based on the iridium(III) complex was reported by Chen and co-workers to be selective for Hcy over Cys and GSH (Figure 2.3). With this probe phosphorescence emission is enhanced in the presence of Hcy and quenched in the case of Cys. Thus, the aldehyde group on this probe reacts with both Hcy and Cys forming thiazinane and thiazolidine adducts respectively. However, the basis for Hcy selectivity was reported to be a result of a photoinduced electron-transfer process on the thiazolidine (Cys adduct). While it's a promising probe, higher concentrations of Hcy  $(400 \mu M)$  were used, by far more than physiological levels. A higher percentage (90%) of the organic solvent (DMSO) was used which would affect the accurate quantitation of analyte in biological samples.<sup>[73](#page-117-0)</sup>



Figure 2.3. Possible recognition mechanism of 9 with Hcy.<sup>[70](#page-116-3)</sup>

Yu *et al*., developed a fluorescent mesoporous silica nanoparticle (MSN) sensor with an anthracene nitroolefin as well as the polyethylene glycol (PEG) covalently immobilized on the particle surface.<sup>[71](#page-116-4)</sup> While all thiols react with the nitroolefin moiety in a Michael addition reaction restoring fluorescence of the anthracene (Figure 2.4), the basis for Hcy selectivity was the PEG molecules that served as a selective barrier blocking other thiols from diffusing into the nanopores. The reported selectivity was achieved at equimolar amounts of thiols (50 µM), 3 times more than plasma levels of tHcy and 6 times less than Cys plasma levels indicating that at physiological levels, Cys would become a major interference. Moreover, at 50  $\mu$ M, it was evident that Cys showed responses that were higher than the control.



Figure 2.4. Proposed mechanism for Hcy selectivity by the Mesoporous silica nanoparticle - based sensor.<sup>[71](#page-116-4)</sup>

Recently, Peng and co-workers reported a redox-based fluorescent probe for selective determination of Hcy (Figure 2.5).<sup>[72](#page-117-1)</sup> The proposed reaction mechanism involves the oxidation of Hcy by a dansyl azide-2 (DN-2) probe selectively over Cys because of the favorable formation of cyclic five-membered ring intermediate as opposed to the strained four membered ring for Cys. The reported selectivity was obtained using equimolar amounts of 100 µM for both Hcy and Cys that do not represent the

physiological levels. Additionally, at 200 µM Cys was found to be interfering with Hcy determination, elevating fluorescence response of probe to Hcy by  $\sim$  40%.



Figure 2.5. Sensing reaction of 13 with Hcy.<sup>[72](#page-117-1)</sup>

Our group developed a visual detection method for Hcy and Cys with aldehydebearing fluorophores based upon the well-known reaction of these thiols to form heterocyclic thiazolidines and thiazinanes.<sup>[74](#page-117-2)</sup> Fluorescence quenching of fluorescein aldehyde probes following the formation of thiazolidine/thiazinane heterocycles with Cys and Hcy was observed under the basic conditions investigated. We further improved this method recently to selectively detect Hcy over Cys by tuning pH and excitation wavelength.<sup>[75](#page-117-3)</sup> At lower pH (5.5-6) and longer wavelength excitations (495 nm), fluorescence enhancement of >5 fold for Hcy over Cys is achieved through inhibition of photo induced electron transfer (PET) as the thiazolidine/thiazinane heterocycles formed become protonated (Figure 2.6).



Figure 2.6. Mechanism of signal transduction in generic aldehyde-bearing amino thiol probes. (a) PETbased fluorescence quenching following reaction of Cys/Hcy with the aldehyde group. (b) PET inhibition through hydrogen bonding between the amine-containing heterocycle and adjacent groups. (c) PET inhibition through protonation of the amine-containing heterocycle.<sup>[75](#page-117-3)</sup>

2.2.3 Hcy selective probes based on free radical chemistry

Biothiols are oxidized to thiyl radicals via three main routes including reaction with carbon centered radicals, with reactive oxygen species (ROS) and through enzymatic oxidation by peroxidases.<sup>[76](#page-117-4)</sup> Two important reactions of thiyl radicals include the reaction with the thiolate to form a reducing disulfide radical anion (Equation 1) and the formation of a reducing alpha-amino carbon-centered radical (Equation 2).

$$
RS^{-} + RS^{\bullet} \longrightarrow RSSR^{\bullet -} (1)
$$

$$
RS^{\bullet} + H_{\vert}^{\vert}RR \rightleftharpoons RSH + {}^{\bullet}\!R R (2)
$$

16

Rate constants of Eq 2 have been reported to be generally of the order of  $10^8 \text{ M}^{-1} \cdot \text{s}^{-1}$  but the reverse reaction is much slower.<sup>[76](#page-117-4)[,77](#page-117-5)</sup> If the hydrogen donation reaction in equation 2, known as the "repair reaction", proceeds intermolecularly, it can promote the "repair" of carbon-centered free radical-containing biomolecules such as carbohydrate-based radicals of DNA.<sup>[76](#page-117-4)</sup> Following the report by Neta and co-workers of the  $\alpha$ -amino alkyl radical of Cys, Sjoberg *et al*. and Zhao *et al*. extended the work and reported the formation of reducing α-amino alkyl radicals of GSH and Hcy through intramolecular rearrangement of their respective thiyl radicals.<sup>[78-80](#page-117-6)</sup>

Importantly, Zhao and co-workers reported that intramolecular formation of the captodatively-stabilized  $\alpha$ -amino alkyl radical in Hcy should be favorable. This was attributed to a kinetically-favored intramolecular hydrogen atom transfer (HAT) mechanism, involving the favored formation of a 5-membered ring in the transition state, as opposed to 4- and 9-membered ring configurations for Cys and GSH, respectively (Figure 2.7). Alpha-amino acid carbon radicals are well-known strong reductants. Captodative stabilization of the alpha-radical renders the alpha C-H bond weaker than the S-H bond by approximately 4 Kcal/mol.



Figure 2.7 Kinetically favored HAT reaction for Hcy. The rate constant for the kinetically-favored sulfurto-carbon-H atom transfer for Hcy is  $>10^5$  s<sup>-1,[80](#page-118-0)</sup>

In their study, Zhao and co-workers used the azide radical to oxidize thiols and the formation of reducing radicals was monitored via UV-Vis absorption spectra of the reduced methyl viologen radical cation  $(MV^{\dagger})$ . Under the highly basic conditions (pH 10.5) investigated by Zhao *et al*., no colorimetric selectivity between GSH, Cys and Hcy was observed. This was due to the presence of significant amounts of thiolate anion promoting the formation of a reducing disulfide radical anion (equation 1) that also reacts with methyl viologen  $(MV^{2+})$  independently of the HAT mechanism. Conversely, neutral conditions investigated by us diminish thiolate formation such that there is only a relatively small percentage of deprotonated thiol. Thus, it was reasoned by our group, that the Hcy-favored HAT process occurring in equation 2 should be more predominant than interfering disulfide radical anion formation at physiological pH. This enabled us to selectively detect Hcy in human blood plasma without any interference from Cys, GSH and other amino acids in  $2004$ .<sup>[74](#page-117-2)[,81](#page-118-1)</sup>

In this colorimetric method remarkable visual color changes were later obtained in human blood plasma without any deproteinization using commercially available  $MV^{2+}$ at neutral pH and reflux conditions (Figure 2.8). The mechanism involves the reduction of  $MV^{2+}$  by the Hcy- $\alpha$ -amino carbon centered radical to its corresponding radical cation which is responsible for the blue color (Figure 2.9). A protocol for visual detection of Hcy was developed based on this method wherein the Hcy thiyl radical is generated by heat.<sup>[82](#page-118-2)</sup> No washing steps, biological reagents or sample pre-processing steps apart from disulfide reduction are needed in this method.



Figure 2.8. Selective detection of Hcy in human plasma spiked with 4.0 mM of Cys, Hcy and GSH, 8.0 mM  $MV^{2+}$ , 0.5 mM Tris buffer pH 7.5, and refluxed for 5 min. Inset shows samples before heating. \*Adapted with permission from the *Journal of the American Chemical Society*, 2005, Volume 127, pages 15949-15958; Weihua Wang, Oleksandr Rusin, Xiangyang Xu, Kyu Kwang Kim, Jorge O. Escobedo, Sayo O. Fakayode, Kristin A. Fletcher, Mark Lowry, Corin M. Schowalter, Candace M. Lawrence, Frank R. Fronczek, Isiah M. Warner, and Robert M. Strongin; Detection of Homocysteine and Cysteine. Copyright 2005 American Chemical Society.



Figure 2.9. Reaction mechanism for selective detection of Hcy using  $MV^{2+}$  at neutral pH<sup>[74](#page-117-2)</sup>. (a) Hydrogen atom transfer (HAT) (b) reduction of  $MV^{2+}(c)$  iminium formation.

While significant progress was made with  $MV^{2+}$ , the probe was only applied to non-reduced plasma and had not been tested in real samples. Human plasma had been spiked with commercial thiol samples. To detect total Hcy (tHcy) a new step had to be introduced, reduction step, to convert all oxidized Hcy species into the reduced form since almost 99% of Hcy is in oxidized disulfide form. Figure 2.10 shows a summary of an improved thermal method that I developed which incorporated the reduction step.



Figure 2.10. Improved thermal method for detection of Hcy.

I investigated this method using non-deproteinized human serum calibration standards (NIST SRM 1955), and successfully distinguished micromolar concentration differences (3.79, 6.13, 13.4 and 38.73  $\mu$ M) of tHcy visually using MV<sup>2+</sup> (Figure 2.11).<sup>[66](#page-116-5)</sup>
As tHcy concentration increased, the color became successively darker and darker as shown by different color shades. The assay protocol involved no sample processing. It only required a two-fold dilution, addition of  $MV^{2+}$  and tris(2-carboxyethyl) phosphine (TCEP), a disulfide reducing agent and 2 min heating at reflux. In this improved method a homogenous solution was formed making it easier to distinguish between different color shades unlike in the previous method where proteins formed clumps upon heating (Figure 2.8).



Figure 2.11. Visual detection of Hcy in human serum calibration standards. Left to right: Hcy concentrations: 3.79, 6.13, 13.4 and 38.7  $\mu$ M respectively.<sup>[66](#page-116-0)</sup>

In order to make the assay potentially more user friendly and benign for potential application at point of care diagnostics and in home test kits, we continued to improve upon the design, synthesis and development of room temperature methods for selective detection of Hcy. Besides the use of heat to promote the reaction, the  $MV^{2+}$  probe is a herbicide and so we investigated the use of less- or non-toxic derivatives. We actually took a two-pronged approach involving the use of photolytic methods described in chapter 3 and the use of novel asymmetric viologen probes described in chapter 4.

# **CHAPTER 3: PHOTOCHEMICAL METHOD FOR SELECTIVE DETECTION OF TOTAL HCY IN PLASMA**

### **3.1 Introduction**

The relatively high costs and complexity of the current methods for Hcy detection have intensified the need to develop selective, yet simple and inexpensive methods that can be used at point of care diagnostics and in home test kits to facilitate the diagnosis and treatment of related diseases. Available kits generally use multi-step washing procedures and/or specialized storage below -20 ºC, limiting their use, for instance, in emerging nations with limited access to refrigeration or electricity. Moreover, even in developed countries point-of-care and kit-based assays are of interest considering rising health care costs and increasing interest in patient-based monitoring.<sup>[83](#page-118-0)</sup>

We hypothesized that photolytic methods would afford analogous selectivity *via*  the intramolecular HAT mechanism while enabling the assay to be carried out at room temperature. Johnson and co-workers reported the photochemical reduction of viologens in ethanolic solutions.  $84$  A mechanism based on the abstraction of a methylene hydrogen atom from EtOH to form a free radical that reduced the viologen in direct sunlight was proposed. We envisioned that this approach could be compatible with our HAT mechanism for Hcy *via* photolytic, rather than thermal generation of the Hcy thiyl radical.

#### **3.2 Results and discussion**

In exploring the use of photolytic methods to detect Hcy, initially we exposed solutions of thiols and  $MV^{2+}$  in Tris buffer at neutral pH to direct sunlight at room temperature. A blue color was observed within 1 minute in the Hcy sample while other thiols solutions remained unchanged (Figure 3.1).



Figure 3.1 Response of  $MV^{2+}$  towards various thiols upon exposure to direct sunlight. Solutions of  $MV^{2+}$ (50 mM) were mixed with thiols (20 µM) in 0.5 M Tris buffer at pH 7, saturated with argon and exposed to sunlight. Pictures were taken at 1 min (left) and 2 min (right) after exposure to sunlight.

To create a laboratory test, we reasoned that an appropriate light source to generate the thiyl radical should emit around 325 nm based on the reported S–H bond dissociation energy of Cys of 370 kJ mol<sup>-1 [85](#page-118-2)</sup> To this end, we selected a very simple and inexpensive compact fluorescent lamp emitting in this region, Reptisun™ consisting of 10% UVB and 30% UVA. The photolysis experiments were performed using this lamp with a light intensity of 6.85 mW  $cm^{-2}$  as measured by a Melles Griot Broadband Power/Energy Meter 13PEM001. We were able to detect Hcy selectively in human blood plasma using  $MV^{2+}$  without any interference from Cys and GSH in the range of their physiological concentrations. Upon irradiation of plasma samples spiked with various biothiols, only the Hcy  $(15 \mu M)$  spiked sample showed significant absorption response whereas Cys and GSH remained unchanged. The absorption spectra are shown in Figure A1, Appendix A.

In previous studies, benzyl viologen  $(BV^{2+})$ , a significantly less toxic chromogen than  $MV^{2+}$ , was found by our group to be more reactive in forming the Hcy  $\alpha$ -amino carbon-centered radical than  $MV^{2+}$  under thermal conditions. BV<sup>2+</sup> has a less negative reduction potential (-370 mV) than  $MV^{2+}$  (-446 mV).<sup>[86](#page-119-0)</sup> Hence we investigated the response of  $BV<sup>2+</sup>$  to Hcy and other thiols using the photochemical method. We observed that  $BV^{2+}$  indeed displayed selectivity towards Hcy under the new photolytic conditions compared to structurally related thiols (Figure 3.2). Moreover, changing the chromogen allowed us to lower its concentration from 50 mM ( $\text{MV}^{2+}$ ) to 20 mM ( $\text{BV}^{2+}$ ). In addition, the Hcy response was greater as compared to photolysis in the presence of  $MV^{2+}$ . An irradiation time of just 15 min afforded optimal selectivity and response.



Figure 3.2 Spectral response of  $BV^{2+}$  towards various spiked thiols in human blood plasma upon irradiation. Absorption spectra of solutions of  $BV^{2+}$  (20 mM) in human blood plasma and 0.5 M Tris buffer (pH 7.0) spiked with 1.5 μM Hcy, 25 μM Cys and 0.6 μM GSH. Plasma (10% v/v) was added to an argonsaturated solution of viologen, thiol & buffer and irradiated for 15 min using a Reptisun<sup>TM</sup> lamp.

Based on the same selectivity pattern and the light source used, the proposed mechanism is assumed to be analogous to the thermal reaction for the selective detection of Hcy we have previously reported.<sup>[74](#page-117-0)</sup> It involves the generation of the Hcy thiyl radical by photolysis followed by the HAT reaction to form the  $\alpha$ -amino carbon centered radical that in turn, reduces  $BV^{2+}$  to its corresponding radical cation  $(BV^{+})$  responsible for the blue color (Figure 3.3).



Figure 3.3 Mechanism for the detection of Hcy involving three steps: (i) photolytic generation of Hcy thiyl radical, (ii) hydrogen atom transfer (HAT) turning the thiyl radical into an α-amino carbon-centered radical, (iii) reduction of  $BV^{2+.83}$  $BV^{2+.83}$  $BV^{2+.83}$ 

Since our ultimate goal was to detect physiological levels of tHcy selectively in human blood plasma, the thiols that are bound to the proteins via disulfide bonds had to be released by reduction. A selective response of  $BV^{2+}$  to Hcy in human plasma was observed after using immobilized tris(2-carboxyethyl)phosphine (TCEP gel), centrifugation and spiking with various thiols (Figure A2, Appendix A).

We optimized the sample processing by replacing the centrifugation step with a simple filtration of the sample through 0.45 µm PVDF filter vials. The spectral response and selectivity was comparable in both methods and excellent selectivity towards tHcy

was observed (Figure 3.4). Interestingly, the use of filters improved the overall background interference from the plasma components.



Figure 3.4 Spectral response of  $BV^{2+}$  towards various spiked thiols in reduced human plasma upon irradiation. Absorption spectra of solutions of  $BV^{2+}$  (20 mM) in reduced human blood plasma and 0.5 M Tris buffer (pH 7.0) spiked with 1.5 μM Hcy, 25 μM Cys and 0.6 μM GSH. Plasma was incubated for 1 h with TCEP Gel followed by filtration using a Single StEP<sup>™</sup> 0.45 μm PVDF filter vial. The reduced, filtered plasma (10% v/v) was added to an argon-saturated solution of viologen, thiol and buffer and irradiated for 15 min using a Reptisun™ lamp.

28 The spectral responses of  $BV<sup>2+</sup>$  to Hcy concentration changes, in spiked reduced human plasma monitored at 615 nm, increased linearly with increasing Hcy concentration over a physiologically relevant concentration range, 0-20 μM with a limit of detection of 3.35 μM (Figure 3.5). The inset shows the respective spectral data. This linear

relationship between absorbance and Hcy concentrations as well as the very low L.O.D makes the assay a potential applicant in the quantitation of tHcy.



Figure 3.5 Spectral response of  $BV^{2+}$  towards increasing levels of spiked Hcy in reduced human plasma upon irradiation. Absorption spectra of solutions of  $BV^{2+}$  (20 mM) in 25% human blood plasma and 0.5 M Tris buffer (pH 7.0) spiked with  $0-5 \mu M$  Hcy. Plasma (25% v/v) was added to an argon-saturated solution of viologen, thiol and buffer, and irradiated for 15 min using a Reptisun™ lamp.

To test the limits of possible Cys and GSH interference with the assay, further experiments were carried out with added excess amounts of Cys and GSH to reduced human plasma solutions. Cys and GSH were found to generate significant response only when their concentrations reach 400  $\mu$ M (almost double the normal concentration in healthy individuals) and 100  $\mu$ M (almost 20 times the normal plasma levels) respectively.

At these concentrations, their absorbance response was equivalent to that of  $5 \mu M$  Hcy (Figure. A3, Appendix A).

To further evaluate the selectivity of the  $BV<sup>2+</sup>$  towards Hcy, control experiments using series of other amino acids were performed. Other amino acids produced no significant absorption response as compared to Hcy, further demonstrating that  $BV^{2+}$  is Hcy specific (Figure 3.6).



Figure 3.6 Spectral response of  $BV^{2+}$  towards various spiked amino acids in human plasma upon irradiation. Absorption spectra of solutions of  $BV^{2+}(20 \text{ mM})$  in human blood plasma and 0.5 M Tris buffer (pH 7.0) spiked with 1.5 µM Hcy and 50 µM amino acids (L-Ala, Arg, Gln, Met, Ser, Thr and Phe). Plasma (10% v/v) was added to an argon-saturated solution of viologen, amino acids and buffer and irradiated for 15 min using a Reptisun™ lamp.

#### **3.3 Experimental section**

#### 3.3.1 Materials and instrumentation

All chemicals were purchased from Sigma-Aldrich and Fisher Scientific and used without further purification. The 0.45 μm Single StEP<sup>TM</sup> PVDF filter vials were purchased from Thomson Instrument Company. UV-visible spectra were acquired on a UV-Vis Cary 50 (Agilent Technologies). The light intensity was measured with a Melles Griot Broadband Power/Energy Meter 13PEM001. The light source for the photolysis experiments was a ReptiSun™ compact fluorescent lamp (Zoo Med Laboratories Inc.).

## 3.3.2 Reduction of Human Blood Plasma

Reconstituted human plasma is incubated with immobilized TCEP gel in a 1:1 volume ratio at room temperature for 1 h with vortexing. Separation of the reduced plasma from the gel can be achieved by centrifugation at 1000 rpm for 5 min or by filtration using a Single StEP™ 0.45 μm PVDF filter vial.

#### 3.3.3 General procedure for the photolysis of thiols in the presence of viologens

In a quartz cuvette sealed with a rubber septum (GL14-S, Starna Cells), a solution of viologen (20 or 50 mM in 0.5 M Tris buffer pH 7.0) is deoxygenated by bubbling Ar for 5 min. Human plasma (spiked or non-spiked) is added to the cuvette and irradiated for 15 min with a Reptisun™ lamp. Absorption spectra are collected on a UV-Vis Cary 50.

The proportion of the plasma solution is 10% of the total volume after being mixed with the viologen solution.

## **3.4 Conclusion**

We have developed a new, relatively simple and inexpensive photochemical assay for the selective detection of total Hcy directly in human blood plasma (Figure 3.7). This method has potential practical application in home test kits or point of care diagnostics because it involves the use of a less toxic chromogen, an inexpensive commercial light source, and simple sample processing, involving only reduction and filtration prior to photolysis and UV-Vis monitoring.



Figure 3.7 Summary of the photochemical method for detection of tHcy.<sup>[83](#page-118-0)</sup>

# **CHAPTER 4: DETECTION OF HCY USING NOVEL ASYMMETRIC VIOLOGEN PROBES**

#### **4.1 Introduction**

After the success we had with benzyl viologen, we envisioned that viologen compounds with higher reduction potentials than benzyl viologen should be more reactive and would not require either heat or light to promote the reaction. Additionally, in another study conducted by our group in collaboration with Crowe and co-workers, the reduction of viologens by α-carbon radicals derived from Hcy and Cys was found to be pH dependent.<sup>[86](#page-119-0)</sup> Symmetric viologens were investigated under reflux conditions and the ones with less negative reduction potentials were more reactive towards amino thiols (Hcy and Cys) at lower pH (Table 4.1). Moreover, these probes were observed to have a faster onset of color formation and more intense color change when the pH was increased beyond the endpoint (minimum pH where color formation was observable).

Based on these findings, we investigated the reaction of phenyl viologen with aminothiols at room temperature. No appreciable reaction was observed and so we were motivated to design viologen probes with even higher reduction potentials. However, there had to be a trade-off between reactivity and selectivity, hence based on the principle that diminished reactivity correlates to higher selectivity, we hypothesized that tuning the redox properties of viologens by making asymmetric probes bearing electron donating and withdrawing groups proximal to the cationic centers would achieve moderate reactivity and allow Hcy to be detected selectively at room temperature without the need for heat or light. To this end, five asymmetric viologen probes (Figure 4.1) were synthesized, characterized and screened for detection of Hcy in biological samples.

<b>Entry</b>	Compound	Reduction potential, (Volts)	pH endpoint of Hcy
$\mathbf{1}$	٠.	$-0.446$	5.0
$\overline{2}$	٠. N	$-0.370$	3.6
3	$\vec{N}$ $\vec{N}$	$-0.288$	2.5

Table 4.1 Reduction potentials of symmetric viologens and pH endpoint of Hcy



Figure 4.1 Structures of novel asymmetric viologen probes

## **4.2 Results and discussion**

#### 4.2.1 Cyclic voltammetry studies

To assess potential electronic effects of different substituents on these asymmetric viologens, cyclic voltammetry studies were carried out in 80 mM phosphate buffer at pH 8 using glassy carbon as the working electrode. As expected, all five probes were observed to have much less negative reduction potentials compared to methyl viologen and behaved as one step redox system (Table 4.2, Figure A5). This implies that these probes should be easier to reduce and more likely at room temperature without the need for heat or light. The trend with increasing reduction potentials (less negative) was found to be: PhCV<sup>2+</sup> (24) < PhNV<sup>2+</sup> (23) < ACNV<sup>2+</sup> (26) < NCV<sup>2+</sup> (25) as expected, due to the increase in the strength of the electron withdrawing substituents (nitrile, coumarin and ester). Compound 27  $(ACNV<sup>2+</sup>)$ , however, deviated from this trend exhibiting a much lesser negative reduction potential than  $ACNV^{2+}$  (26) even though the nitrile or cyano is a more powerful electron withdrawing group than the coumarin. This could have been due to the precipitation we observed in this system and this probe also suffered some adsorption.

At the scan rate of 50 mV/s, viologen probes **26** and **24** voltammograms displayed some quasi-reversibility of their reaction systems. This was further confirmed at both higher (100 mV/s) and lower scan rates (10 mV/s). The quasi-reversibility may have been a result of slow charge transfer processes or the dication may have been further reduced to its fully reduced state.<sup>[87](#page-119-1)</sup> It has also been reported that the formation of spin-paired radical cation dimers can cause quasi-reversibility of reduction systems.<sup>[88](#page-119-2)</sup>

<b>Entry</b>	Compound	<b>Vs NHE (Volts)</b>
1	Methyl viologen $(MV^{2+})$	$-0.404$
2	$PhCV^{2+}$ (24)	$-0.188$
3	PhNV <sup>2+</sup> (23)	$-0.161$
4	$ACNV^{2+}(26)$	$-0.133$
5	$ACCV^{2+}(27)$	$-0.123$
6	$NCV^{2+}(25)$	$-0.118$

Table 4.2: Reduction potentials of novel asymmetric viologens vs methyl viologen

#### 4.2.2 Reactivity with amino thiols

All five probes were screened for their optical sensing behavior towards the amino thiols Hcy, Cys and GSH. Screening was done at rt, higher concentrations of thiols (1 mM), probe (4 mM) and in various buffers at different pH conditions (phosphate pH 6, 7 and 8; Tris pH 7, 8 and 9; Hepes pH 7 and 8). PhCV<sup>2+</sup> (25) produced excellent selectivity towards GSH and this is described in detail in chapter 5.  $ACCV<sup>2+</sup>$  (27) was selective for Hcy at higher concentrations of the thiols (1mM). At pH 8 (phosphate buffer, 80 mM), probe **27** developed an intense color upon reaction with Hcy whereas Cys and GSH samples had the same color as the blank (Figure 4.2). Attempts to lower the thiol concentration below 1 mM resulted in loss of Hcy selectivity and all thiols developed the same color as the blank.



Figure 4.2 Response of ACCV<sup>2+</sup> (27) towards various amino thiols at pH 8. ACCV<sup>2+</sup> (4 mM) was added to thiol solutions (1 mM each) buffered at pH 8 (phosphate buffer (80 mM). From left to right: Blank, Hcy, Cys and GSH. The picture was taken 30 min after mixing solutions at room temperature.

UV-Vis absorption spectroscopy was used to monitor the reaction between the asymmetric probes and biological thiols. As shown in Figure 4.3, upon mixing solutions of NCV<sup>2+</sup> (25) with amino thiols in phosphate buffer (80 mM) at pH 8, a significant color

change was observed in the sample containing Cys after 5 min. However, no significant color formation or absorption response was seen in the case of Hcy or GSH samples. Over time, Hcy was found to promote a signal. This is in agreement with our earlier study under reflux conditions where we found that at higher pH, the colorimetric response of symmetric viologen probes towards  $\alpha$ -carbon radicals from both Hcy and Cys becomes less Hcy selective.



Figure 4.3 Spectral response of NCV<sup>2+</sup> (25) towards various amino thiols at pH 8. Absorption spectra of solutions of NCV<sup>2+</sup> (4 mM) in thiol solutions (1 mM) buffered at pH 8 (phosphate buffer (80 mM). The inset shows the picture taken at 10 min.

We investigated the reaction of  $ACNV^{2+}$  (26) with Hcy, Cys and GSH in 80 mM phosphate buffer (pH 8) and found that Hcy can be detected selectively under these conditions without interference from related analytes. Through optimization of the reaction, we were able to distinguish Hcy from Cys and GSH at their physiological levels in natural media. Upon adding  $26$  (350  $\mu$ M) to solutions of Hcy (15  $\mu$ M), Cys (250  $\mu$ M) and GSH (6 μM) buffered at pH 8 (phosphate buffer, 80 mM), a marked color change as well as an intense absorption response was observed for the Hcy solution.

While monitoring the change in absorbance at 547 nm as a function of time (Figure 4.4) over 2 to 10 min, it was observed that Hcy can be detected selectively without any significant interference from both Cys and GSH. Thereafter, Cys reacts in an opposing fashion to that of Hcy showing a decreased absorbance peak, far below that of both the blank and GSH. The Cys solution peak began to diminish after 10 min, showing a plateau at 25 min. Thus, Hcy can be detected selectively without interference from Cys and GSH at their physiological levels at 10 min (Figure A4, Appendix A).



Figure 4.4 Time-dependent spectral response of  $ACNV^{2+}$  (26) towards various amino thiols at pH 8. Timedependent absorbance changes of **26** (350 μM) in thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (Phosphate buffer, 80 mM). The inset shows the picture taken at 30 min.

The absorption spectra displaying opposing reaction behaviors of **26** towards Hcy and Cys are shown in Figure 4.5. In the case of Cys the absorbance band at 547 nm decreased with concomitant growth of the band at 400 nm over time (Figure 4.5b) whereas for Hcy both bands increased with time (Figure 4.5a). This is the first example, to our knowledge, of a redox-based probe that detects Hcy and Cys simultaneously at typical biological levels found in human plasma.



Figure 4.5 Optical sensing behavior of  $ACNV^{2+}$  (26) towards Hcy and Cys at pH 8. (a) Absorption spectra of **26** with Hcy (15 μM) over 30 min. (b) Absorption spectra of **26** with Cys (250 μM) over 30 min.

From the screening studies,  $PhNV^{2+}$  (23) was found to be the most promising probe for detecting Hcy selectively at rt at its physiologically relevant levels. The reaction of **23** (2.5 mM) with Hcy (15  $\mu$ M), Cys (250  $\mu$ M) and GSH (6  $\mu$ M) at rt, pH 8 was investigated by monitoring the changes in absorbance at 550 nm as a function of time. Hcy induced a fast response and the absorbance increased rapidly up to about 10 min and then just gradually thereafter (Figure 4.6). As for Cys and GSH solutions, their absorbance changes over 25 min overlapped with the blank demonstrating that this probe is Hcy specific.

After several hours all the thiols become indistinguishable as the absorbance increase due to Hcy, converges with the absorbance levels from GSH and Cys.



Figure 4.6 Time-dependent spectral response of  $PhNV^{2+}$  (23) towards various amino thiols at pH 8. Timedependent absorbance changes of **23** (2.5 mM) in thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (phosphate buffer, 80 mM).

Based on these findings, we selected 10 min as the optimal reaction time for further studies monitoring at 550 nm. The corresponding absorption spectra at 10 min showed high selectivity for Hcy, however there was a change via emergence of a peak between 400 and 450 nm, showing the blank and Cys increasing relatively slightly (Figure 4.7).



Figure 4.7 Spectral response of PhNV<sup>2+</sup> (23) towards various amino thiols at pH 8. Absorption spectra of **23** (2.5 mM) in thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (phosphate buffer, 80 mM) after 10 min.

Upon lowering the probe concentration to 2 mM, in the presence of thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (phosphate buffer, 80 mM), **23** developed a strong pink color and generated a significant absorbance response for Hcy without any interference from Cys and GSH (Figure 4.8). Samples containing Cys and GSH developed the same color as the blank and their absorption spectra overlapped.



Figure 4.8 Spectral response of PhNV<sup>2+</sup> (23) towards various amino thiols at pH 8. Absorption spectra of solutions of PhNV<sup>2+</sup> (2 mM) in thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (phosphate buffer (80 mM). The inset shows the picture taken at 10 min.

The reaction profile of **23** towards amino thiols further confirmed the specificity of the probe for Hcy as shown by the rapid increase in absorbance relative to that of Cys, GSH and the blank. The absorbance changes for Cys and GSH increased steadily in the same manner as the blank and produced no interference to Hcy over the 15 min period the reaction was monitored (Figure 4.9).



Figure 4.9 Time-dependent spectral response of  $PhNV^{2+}$  (23) towards various amino thiols at pH 8. Timedependent absorbance changes of **23** (2 mM) in thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (phosphate buffer, 80 mM).

To enable quantitative determination of Hcy, experiments were conducted to evaluate the sensing behavior of **23** upon increasing the concentration of Hcy. It can be observed in Figure 4.10 that the absorbance changes of **23** versus Hcy concentration changes at 550 nm increased linearly proportional to increasing Hcy concentration over a physiologically relevant concentration range (0-25 μM) with a very limit of detection of 2.04 μM. The inset shows the corresponding spectral data.



Figure 4.10 Concentration dependent responses of **23** (2 mM) towards Hcy. A Calibration curve for Hcy showing a linear relationship between absorbance at 550 nm and Hcy concentration (0-25 μM) at pH 8 (Phosphate buffer, 80 mM). The inset shows the absorption spectra of probe **23** upon addition of increasing Hcy concentrations.

The applicability of **23** in a complex biological system was evaluated using commercial human plasma. Upon addition of the probe directly to plasma solutions, a very dark pink color developed showing that the probe reacted with proteins. The plasma was then deproteinized and, after addition of **23** to plasma samples spiked with various amino thiols (15 μM Hcy, 250 μM Cys and 6 μM GSH) at pH 8 (phosphate buffer, 80 mM), only the Hcy spiked sample displayed significant absorption response whereas Cys and GSH spiked solutions responded in the same manner as the blank (Figure 4.11). In deproteinized plasma, the probe functioned similarly as in aqueous conditions; however, a decrease in the absorbance change was observed as a result of matrix effects. The selective response of **23** to Hcy over Cys and GSH in plasma combined with the

simplicity of the probe makes it a potential indicator for use in testing Hcy at point of care and in a home setting.



Figure 4.11 Spectral response of PhNV<sup>2+</sup> (23) towards various spiked thiols in deproteinized human plasma (dep plasma). Absorption spectra of solutions of  $PNV^{2+}$  (2 mM) in human blood plasma (10% v/v) spiked with various thiols (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (phosphate buffer (80 mM). The inset shows the picture taken at 10 min.

## 4.2.3 Mechanistic studies

To evaluate whether a free radical mechanism was responsible for Hcy selectivity using the asymmetric probes at room temperature or not, Electron paramagnetic Resonance (EPR) spectroscopy was performed in the absence and presence of analytes. EPR is spectroscopic technique that is used to detect, distinguish and quantify different reactive species hence, it plays a pivotal role in the investigations of redox-mediated chemical reactions.

46 As expected, the involvement of radicals in probe reactivity was confirmed by the EPR spectra (Figure 4.12). However, in the absence of Hcy, the probe itself generated

a radical of high amplitude, an indication of a higher concentration of resonating paramagnetic species in the sample. The reduction in the probe EPR amplitude in the presence of Hcy suggests that Hcy promoted the formation of more radicals which consequently formed radical cation dimers. These radical cation dimers are diamagnetic hence they do not give an EPR signal.  $89-91$  What was not clear from EPR studies is whether the mechanism involves hydrogen atom transfer (HAT) which is more favorable for Hcy or some other radical addition process.



Figure 4.12 EPR spectra of PhNV<sup>2+</sup> (23), (20 mM) in the presence and absence of Hcy (10 mM) at pH 8 (80 mM, phosphate buffer).

HAT process occurred selectively for Hcy at neutral pH, but at higher pH the formation of interfering disulfide radical anions from each thiol renders the method nonselective. However, at pH 8 using the asymmetric probes, we were able to detect Hcy selectively. From our investigations using 2-mercaptoethanol (BME) and 3 mercaptopropionic acid (MPA), the involvement of HAT cannot be ruled out. BME and

MPA are very similar to Hcy in the sense that they possess an –SH group bearing two methylene groups but they are not capable of producing the  $\alpha$ -amino carbon centered stabilized radicals. As shown in Figure 4.13, only the sample containing Hcy turned dark red while BME and MPA samples turned yellowish. This suggests that the  $\alpha$ -amino carbon centered radical is involved in the sensing mechanism.



Figure 4.13. Response of PhNV<sup>2+</sup> (23) towards Hcy, MPA and BME. All solutions were composed of 23 (2) mM), analytes (Hcy, MPA and BME, 100 μM) in 80 mM phosphate buffer, pH 8. Pictures were taken at 30 min.

## **4.3 Experimental section**

#### 4.3.1 Materials and instruments

48 All chemicals were purchased from Sigma-Aldrich or Acros Organics and used without further purification.<sup>1</sup>H-NMR and <sup>13</sup>C-NMR spectra were recorded on a Bruker AMX-400 NMR spectrometer, using TMS as an internal standard. Chemical shifts (δ) are given in ppm relative to DMSO- $d_6$  (2.50 ppm, <sup>1</sup>H, 39.52<sup>-13</sup>C) unless otherwise indicated.

ESI-HRMS (electrospray ionization - high resolution mass spectrometry) spectra were obtained on a Thermo Electron LTQ Orbitrap hybrid mass spectrometer with a dedicated Accela HPLC system. Electrochemical measurements were performed with a Gamry Reference 600 potentiostat. A three-electrode system was used, consisting of a glassy carbon working electrode, a platinum wire counter electrode and a Ag/AgCl reference electrode. Reduction potentials were determined using the half wave reduction potential. EPR studies were performed using a Bruker (Fremont, CA) EMX spectrometer equipped with a high-sensitivity cavity and an Aqua-X sample holder. Spectra were obtained at room temperature. UV-visible spectra were collected on a Cary 50 UV-Vis spectrophotometer and pH measurements were carried out with an Orion 410A pH meter.

4.3.2 Synthesis of asymmetric viologen probes

# **Phenyl-nitrile viologen, PhNV2+ (23)**



Figure 4.14 Synthesis of phenyl-nitrile viologen,  $PhNV^{2+}$  (23)

# **1-(2,4-Dinitrophenyl)-4,4'-bipyridin-1-ium chloride (32)** [92](#page-119-4)

The synthetic procedure was adapted from work by Coe and co-workers but under anhydrous conditions.<sup>[92](#page-119-4)</sup> Under Ar, 4,4'-bipyridine **30** (2 g, 12.81 mmol) is dissolved in 10 mL of anhydrous EtOH. To this solution is added 2,4-dinitrochlorobenzene **31** (2.59 g, 12.81 mmol) in 10 mL EtOH dropwise and refluxed for 24 h. The mixture is cooled to rt and added to diethyl ether (200 mL) with stirring. The resulting golden-brown precipitate is filtered, washed with diethyl ether and dried under vacuum in an argon-saturated glove box to give a light brown solid (3.519 g, 85%). <sup>1</sup>H NMR (400 MHz, DMSO) δ 9.66 (d, *J* = 7.0 Hz, 2H), 9.14 (d, *J* = 2.5 Hz, 2H), 9.05 – 8.97 (m, 3H), 8.94 (dd, *J* = 4.5, 1.6 Hz, 2H), 8.52 (d, *J* = 8.7 Hz, 1H), 8.23 (dd, *J* = 4.5, 1.7 Hz, 2H).

# **1-(Phenyl)-4,4'-bipyridin-1-ium hexafluorophosphate (34)** [93,](#page-120-0)[94](#page-120-1)

Procedures published by Kamogawa *et al*. and Carballada *et al.* were modified to synthesize compound **34.** Compound **32** (1 g, 2.79 mmol) is dissolved in EtOH (20 mL) by gentle heating at >60 ºC. A solution of aniline (**33**) (1.27 mL) in 10 mL EtOH is added dropwise and the mixture is stirred at rt for 24 h. The solvent is removed *in vacuo* and diethyl ether (100 mL) added to the residue. This is followed by stirring at rt for 30 min and then filtering off the solution. This is repeated two more times until the filtrate is clear and the resulting dark-red residue is heated in  $H_2O$  (50 mL) for 24 h. An aqueous solution of 1 M  $NH_4PF_6$  is added to the filtrate dropwise to give a pale yellow precipitate which is filtered, washed with water and dried under vacuum (0.693 g, 66%). <sup>1</sup>H NMR

(400 MHz, DMSO)  $\delta$  9.53 – 9.49 (m, 2H), 8.92 (d, J = 6.0 Hz, 2H), 8.81 – 8.77 (m, 2H), 8.15 (dd, J = 4.5, 1.7 Hz, 2H),  $7.96 - 7.91$  (m, 2H),  $7.80 - 7.76$  (m, 3H).

# **Phenyl-nitrile viologen, PhNV2+ (23)**

Under argon, compound **36** (0.200 g, 0.529 mmol) and bromoacetonitrile (0.368 mL, 5.29 mmol) are dissolved in 20 mL of anhydrous acetonitrile (MeCN). The mixture is heated to reflux for 24 h and cooled to rt. The resulting precipitate is filtered, washed with fresh MeCN, and dried under vacuum to yield a yellow powder (0.0985 g, 43%). <sup>1</sup>H NMR (400 MHz, DMSO):  $\delta$  9.69 (d, J = 7.0 Hz, 2H), 9.50 (d, J = 7.0 Hz, 2H), 8.95 (dd, J  $= 9.9, 7.0$  Hz, 4H),  $7.98 - 7.94$  (m, 2H),  $7.82 - 7.79$  (m, 3H), 6.05 (s, 2H). <sup>13</sup>C NMR (101) MHz, DMSO) δ 150.06, 149.02, 146.59, 145.96, 142.23 131.63, 130.26, 127.18, 126.66, 124.81, 114.14 47.80. HR ESI [M - H]<sup>+</sup>, m/z: 272.1188; calc for C<sub>18</sub>H<sub>14</sub>N<sub>3</sub><sup>2+</sup>; 272.1187,  $[M - C<sub>2</sub>H<sub>2</sub>N]$ <sup>+</sup>, m/z: 233.1079 calc for  $C<sub>16</sub>H<sub>13</sub>N<sub>2</sub><sup>+</sup> 233.1077$ .

**Phenyl-coumarin viologen**, **PhCV 2+ (24)**



Figure 4.15 Synthesis of phenyl-coumarin viologen, **PhCV 2+ (24)**

51 Under argon, compound **34** (0.200 g, 0.529 mmol) and 3-(bromoacetyl) coumarin **35** (0.706 g, 2.64 mmol) are dissolved in 20 mL of anhydrous MeCN. The mixture is heated to reflux for 24 h and cooled to rt. The resulting precipitate is filtered, washed with fresh MeCN, acetone and dried under vacuum to yield a yellow powder (0.187 g, 61%). <sup>1</sup>H NMR (400 MHz, DMSO): δ 9.74 (d, *J* = 6.5 Hz, 2H), 9.32 (d, *J* = 6.4 Hz, 2H), 9.04-9.00 (m, 5H), 8.13 (d, *J* = 7.0 Hz, 1H), 8.00 (d, *J* = 3.7 Hz, 2H), 7.89 (t, *J* = 7.8 Hz, 1H), 7.83 – 7.78 (m, 3H), 7.61 (d, *J* = 8.4 Hz, 1H), 7.52 (t, *J* = 7.5 Hz, 1H), 6.48 (s, 2H). <sup>13</sup>C NMR (101 MHz, DMSO) δ 187.59, 158.79, 154.89, 149.60, 147.23, 145.94, 142.15, 135.98, 131.54, 130.25, 126.53, 125.57, 124.93, 121.12, 117.98, 116.47, 68.95. HR ESI [M-H]<sup>+</sup>, m/z: 419.1396; calc for  $C_{27}H_{19}N_2O_3^{2+}419.1374$ , [M+OH]<sup>+</sup> m/z: 437.1457 calc for  $C_{27}H_{20}N_2O_4^{2+}$ 437.1478, [M –  $C_{11}H_7O_3$ ]<sup>+</sup>, m/z: 233.1079 calc for  $C_{16}H_{13}N_2^{+}$ 233.1066, [M+2H]<sup>2+</sup> m/z: 420.1474 calc for  $C_{27}H_{20}N_2O_3^{2+}210.0726$ .

**Nitrile-Coumarin viologen**, **NCV 2+ (25)**



Figure 4.16 Synthesis of Nitrile-coumarin viologen,  $NCV^{2+}$  (25).

#### **1-(2-oxo-2-(2-oxo-2H-chromen-3-yl)ethyl)-[4,4'-bipyridin]-1-ium bromide (36)**

Compound 36 is synthesized following a procedure reported by our group.<sup>[95](#page-120-2)</sup> 4,4'bipyridine **30**, (1.46 g, 9.36 mmol) and 3-(bromoacetyl)coumarin **37** (1 g, 3.74 mmol) are dissolved in 40 mL of acetone and stirred at rt for 3 h. The precipitate is filtered, washed with acetone and dried under vacuum to give a purple precipitate  $(1.279 \text{ g}, 81\%)$ . <sup>1</sup>H NMR (400 MHz, DMSO): δ 9.13 (d, *J* = 6.9 Hz, 2H), 9.02 (s, 1H), 8.91 (dd, *J* = 4.5, 1.6 Hz, 2H), 8.77 (d, *J* = 7.0 Hz, 2H), 8.15 – 8.08 (m, 2H), 7.92 – 7.84 (m, 1H), 7.61 (d, *J* = 8.4 Hz, 1H), 7.52 (t, *J* = 7.5 Hz, 1H), 6.39 (s, 2H).

# **Nitrile-coumarin viologen, NCV2+ (25)**

53 The hexafluorophosphate salt (**37**) was prepared by dissolving the bromide salt **(36)** in water (15 mL) followed by dropwise addition of an aqueous solution of 1 M  $NH_4PF_6$  until a solid precipitated completely. The light purple precipitate is filtered, washed with H2O and dried under vacuum. Under argon atmosphere, compound **33** (0.200 g, 0.410 mmol) and bromoacetonitrile (0.286 mL, 4.10 mmol) are dissolved in 20 mL of anhydrous acetonitrile (MeCN). The mixture is heated to reflux for 5 h and cooled to rt. The resulting yellow precipitate is filtered, washed with fresh MeCN, recrystallized from EtOH and dried under vacuum to yield a yellow powder  $(0.125 \text{ g}, 56\%)$ . <sup>1</sup>H NMR (400 MHz, DMSO): δ 9.53 (d, *J* = 7.0 Hz, 2H), 9.26 (d, *J* = 7.0 Hz, 2H), 9.01 (s, 1H), 8.90 (t, *J* = 7.0 Hz, 4H), 8.12 (dd, *J* = 7.9, 1.5 Hz, 1H), 7.92 – 7.86 (m, 1H), 7.61 (d, *J* = 8.4 Hz, 1H), 7.52 (dd, *J* = 11.7, 4.3 Hz, 1H), 6.43 (s, 2H), 6.10 (s, 2H). <sup>13</sup>C NMR (101 MHz, DMSO) δ 187.83, 158.67, 154.90, 150.43, 149.73, 147.30, 146.50, 136.02, 131.59,

127.16, 126.48, 125.56, 121.10, 117.94, 116.40, 114.10, 69.09, 47.76. HR ESI [M-H]<sup>+</sup> m/z: 382.1181 calc for  $C_{23}H_{16}N_3O_3^{2+}$  382.1175.

# **Acetyl-nitrile viologen, ACNV 2+ (26)**

Compound **26** was synthesized using microwave irradiation by modifying the method used by Lambert and co-workers to synthesize asymmetric viologens.<sup>[96](#page-120-3)</sup>



Figure 4.17 Synthesis of Acetyl-nitrile viologen,  $ACNV^{2+}$  (26)

## **1-(acetoxymethyl)-[4,4'-bipyridin]-1-ium bromide (41)**

4,4'-bipyridine **30**, (0.500 g, 3.20 mmol) and bromomethylacetate (0.157 mL, 1.60 mmol) are dissolved in 4.00 mL of anhydrous DCM in a sealed microwave vial equipped with a stir bar. The mixture is irradiated on a Biotage Initiator at 60  $\degree$ C for 1 h. The vial is cooled to rt and the resulting precipitate is filtered, washed with fresh DCM and dried under vacuum overnight to give a very pale yellow solid (0.653 g, 66 %).

<sup>1</sup>H NMR (400 MHz, DMSO):  $\delta$  9.34 (d, *J* = 7.0 Hz, 2H), 8.89 (d, *J* = 6.0 Hz, 2H), 8.69 (d,  $J = 7.0$  Hz, 2H), 8.05 (dd,  $J = 4.5$ , 1.7 Hz, 2H), 6.45 (s, 2H), 2.17 (s, 3H). <sup>13</sup>C NMR (101 MHz, DMSO) δ 169.72, 154.57, 151.03, 145.67, 140.67, 125.32, 122.03, 78.85, 20.57. HR ESI [M-H]<sup>+</sup>, m/z: 229.0977; calc for  $C_{13}H_{13}N_2O_2^+$  229.0969.

# **Acetyl-nitrile viologen, ACNV2+ (26)**

The hexafluorophosphate salt (**40**) was prepared following the procedure used for compound **37** above. Compound **40** (0.100 g, 0.268 mmol) and bromoacetonitrile (0.186 mL, 2.68 mmol) are dissolved in 4.00 mL of anhydrous MeCN in a sealed microwave vial equipped with a stir bar. The mixture is irradiated on a Biotage Initiator at  $100^0C$  for 30 min. The vial is cooled to rt and the resulting precipitate filtered, washed with fresh DCM and dried under vacuum overnight to give a green-yellowish solid (0.047 g, 41 %). <sup>1</sup>H NMR (400 MHz, DMSO): δ 9.57 – 9.46 (m, 4H), 8.86 (dd, *J* = 14.3, 6.6 Hz, 4H), 6.51 (s, 2H), 6.09 (s, 2H), 2.18 (s, 3H). <sup>13</sup>C NMR (101 MHz, DMSO)  $\delta$  169.48, 150.32, 146.31, 127.01, 114.03, 79.31, 47.71, 20.56. HR ESI [M-H]<sup>+</sup> , *m/z*: 268.1086 calc for  $C_{15}H_{14}N_3O_2^{2+}$  268.1077, [M – C<sub>2</sub>H<sub>2</sub>N]<sup>+</sup>, *m/z*: 229.0977; calc for  $C_{13}H_{13}N_2O_2^{+}$  229.0969,  $[M + CH<sub>3</sub>]$ <sup>+</sup>, *m/z*: 283.1321 calc for 283.1128

**Acetyl-Coumarin viologen, ACCV 2+ (27)**



Figure 4.18 Synthesis of Acetyl-coumarin viologen,  $ACCV<sup>2+</sup>$  (27).

Under Ar, 3-(bromoacetyl) coumarin **35** (0.358 g, 1.34 mmol) was dissolved in 15 mL of anhydrous MeCN and heated to reflux. A solution of compound **40** (0.100 g, 0.268 mmol) in 10 mL anhydrous MeCN is added dropwise and the mixture is refluxed for 5 h. After cooling to rt, the resulting precipitate is filtered, washed with fresh MeCN and dried under vacuum to yield an orange powder  $(0.0618 \text{ g}, 39\%)$ . <sup>1</sup>H NMR  $(400 \text{ MHz}, \text{DMSO})$ : δ 9.55 (d, *J* = 6.9 Hz, 2H), 9.29 (d, *J* = 6.9 Hz, 2H), 9.02 (s, 1H), 8.92 (t, *J* = 7.0 Hz, 4H), 8.12 (dd, *J* = 7.8, 1.4 Hz, 1H), 7.92 – 7.85 (m, 1H), 7.61 (d, *J* = 8.4 Hz, 1H), 7.52 (dd, *J* = 11.6, 4.2 Hz, 1H), 6.54 (s, 2H), 6.46 (s, 2H), 2.19 (s, 3H). <sup>13</sup>C NMR (101 MHz, DMSO)  $\delta$ 187.74, 169.56, 158.74, 154.72, 150.99, 149.81, 149.08, 147.20, 146.03, 136.14, 131.67, 126.72, 125.56, 121.09, 117.76, 116.35, 79.18, 69.05, 20.52. HR ESI [M-H]<sup>+</sup> , *m/z*: 415.1294 calc for  $C_{24}H_{19}N_2O_5^{2+}$  415.1279,  $[M+OH]^+$ ,  $m/z$ : 433.1389 calc for  $C_{24}H_{21}N_2O_6^{2+}$  433.1384, [M-C<sub>3</sub>H<sub>6</sub>O<sub>2</sub>]<sup>+</sup>, *m/z*: 343.1077; calc for  $C_{21}H_{15}N_2O_3^{+}$  341.1073,  $[M-C_{10}H_6O_3]^+$ , *m/z*: 243.1134; calc for  $C_{14}H_{15}N_2O_2^+$  243.1124.
4.3.3. Cyclic voltammetry

Glassy carbon working electrodes were polished with 0.05 µm alumina Struers OP-Alumina suspension on a Buehler microcloth, followed by sonication in deionized  $H_2O$ . All electrochemical cyclic voltammograms used a Pt flag counter electrode  $(1 \text{ cm}^2)$ and a Ag/AgCl reference electrode. The electrode was immersed in an aqueous solution a viologen (4 mM) buffered at pH 8 and cycled at a rate of 10, 50 or 100 mV/s. All experiments were performed at ambient temperature.

4.3.4 General procedure for the UV/Vis absorption responses of asymmetric viologen probes towards thiols.

The probe was added to solutions of thiols in buffer at pH 8.0 (phosphate buffer, 80 mM) and vortexed for about 5 seconds to ensure thorough mixing. The solution was then pipetted into a cuvette for UV-Vis spectra collection. In the case of deproteinized plasma, its proportion was 10% of the total volume after being mixed with buffer and probe solutions. Deproteinized plasma was obtained by reconstituting lyophilized commercial human plasma with Milli-Q® grade water to 1/3 of the reconstitution volume. Proteins were then precipitated using MeCN (two thirds of the reconstitution volume) followed by centrifugation at 4,000 rpm for 30 min. The supernatant liquid was decanted, lyophilized for 12 h and stored at 4 ºC for further use.

# **4.4 Conclusion**

We have developed novel redox-based asymmetric viologen probes that can selectively detect Hcy, Cys and GSH without any interference from each other. **PhNV 2+ (23)** and  $\text{ACNV}^{2+}$  (26) have been proved to be sensitive probes that can detect Hcy selectively at relevant plasma concentrations, which are significantly lower compared to the concentration of competing analytes such as Cys. Additionally, a linear calibration curve obtained for **23** with increasing Hcy concentration over a physiologically relevant range (0-25 μM) with a very low L.O.D of 2.04 μM demonstrating a high potential for quantitation of total Hcy in complex biological samples.

### **CHAPTER 5: SELECTIVE DETECTION OF GSH USING OPTICAL PROBES**

### **5.1 Significance of glutathione to public health**

GSH plays a significant role in the detoxification of free radicals and reactive oxygen species (ROS) thus maintaining and regulating the redox status of cells.<sup>[97](#page-120-0)[,98](#page-120-1)</sup> Diminished levels of GSH which manifest largely through an increased susceptibility to oxidative stress are characteristic of chronic diseases. Chronic diseases are characterized by long duration and relatively slow progression and include heart disease, stroke, cancer, chronic respiratory diseases and diabetes. They are the leading cause of mortality in the world, accounting for approximately 63% of all deaths. $\frac{99}{2}$  $\frac{99}{2}$  $\frac{99}{2}$ 

Results published in 1999 by Beutler E. *et al*., revealed a decrease in erythrocyte GSH content in patients affected by γ-glutamylcysteine synthetase deficiency and hemolytic anemia.<sup>[100](#page-120-3)</sup> Recently, Atkuri and co-workers reported intracellular reduced glutathione (GSH) deficiency in mitochondrial disorders and organic acidemias.<sup>[101](#page-121-0)</sup> Mitochondrial disorders can cause organ failure, seizures, stroke-like episodes and premature death. Depleted intracellular GSH levels were also reported in various neurodegenerative disorders such as Alzheimer's and Parkinson's disease.<sup>[102](#page-121-1)[,103](#page-121-2)</sup> Oxidative stress is the major proposed pathogenic mechanism for neurodegenerative disorders in which mitochondrial defects have been reported. GSH monitoring is a promising new means to diagnose mitochondrial disorders and in clinical trials to monitor autism by indexing the imbalance of oxidative and anti-oxidative stress systems in

autistic patients. [101](#page-121-0) Mancuso *et al*. reinforced the same findings that oxidative stress biomarkers which include GSH may be useful in the detection of redox imbalance in mitochondrial diseases and provision of non-invasive tools for monitoring disease status.<sup>[104](#page-121-3)</sup> Whole blood GSH measurements have also been used to monitor the responses of patients to glutamine (GLN) therapy following open heart surgery.<sup>[105](#page-121-4)</sup>

Conversely, elevated GSH levels generally increase antioxidant capacity and resistance to oxidative stress, and this is observed in many types of cancer cells.<sup>[98](#page-120-1)</sup> Higher levels of GSH have been reported in a number of different human cancer tissues including, bone marrow, breast, colon and  $\mu$ <sub>ngs</sub>.<sup>[106-108](#page-121-5)</sup> While GSH is important in the detoxification of carcinogens, its elevated state in cancerous cells and solid tumors makes them more resistant to chemo- and radiotherapy.<sup>[109](#page-122-0)</sup>

### **5.2 Current methods for GSH detection**

Current diagnostic methods require a separation step (chromatographic<sup>[110](#page-122-1)</sup>), fragile materials (that need skilled handling and specialized storage) and intensive sample processing.<sup>[111,](#page-122-2)[112](#page-122-3)</sup> Various useful innovative indicators and probes for GSH detection have been recently reported. However, many of them have no specificity for GSH over other structurally similar, competing thiols.<sup>[113-116](#page-122-4)</sup> Many reports for instance, claim GSH selectivity via fluorescent indicators, however, close scrutiny often reveals that the stated selectivity suffices only in specific applications such as cell imaging, and that Cys, Hcy and other sulfhydril-containing species interfere with the purported GSH indicators.<sup>[113-116](#page-122-4)</sup>

Lim *et al*., reported an activated coumarin-3-phenyl enone fluorescent probe, **41** which responded selectively and ratiometrically to GSH and Cys over other natural amino acids through the Michael addition reaction.<sup>[114](#page-122-5)</sup> However, their results showed a significant response from Cys although the GSH response was greater. Additionaly, Hcy another structurally related analyte which could potentially interfere with the system was not investigated using this probe. Since the mechanism involves a Michael addition reaction of the probe to the thiol group, this probe will react with all thiols making it nonspecific for GSH only. Higher concentrations of GSH of 20 mM were used which do not reflect the physiological levels in both plasma and blood cells.



Figure 5.1. Michael addition reaction of 41 with thiols.<sup>[114](#page-122-5)</sup>

Another non-specific thiol probe, 1,3,5,7-tetramethyl-8-phenyl-(2-maleimide) difluoroboradiaza-s-indacene, (TMPAB-o-M) was shown to respond to *N*-acetylcysteine and used for labeling BSA in SDS-PAGE.<sup>[117](#page-123-0)</sup> Subsequently, the same probe was applied in the selective spectrofluorometric determination of glutathione in clinical and biological samples.<sup>[118](#page-123-1)</sup> Due to the probe's lack of specificity, complex sample preparation and a separation step were needed to help detect GSH selectively.

There are very few indicators that achieve good selectivity for GSH over other biological thiols. However, some of them have only been applied in cells where GSH concentrations are higher (1-2 mM) but have not been applied in plasma where where its concentrations are very low (1-6  $\mu$ M) compared to those of Cys (135–300  $\mu$ M) and Hcy (5–15  $\mu$ M). <sup>[6](#page-107-0)[,7](#page-107-1)[,10](#page-108-0)[,16](#page-109-0)</sup> Examples include a monochlorinated BODIPY-based ratiometric fluorescent sensor developed by Niu and co-workers, <sup>[116](#page-123-2)</sup> a bis-spiropyran ligand developed for cellular imaging,  $119$  a quantum-dot-based off-on fluorescent probe  $120$  and cyanine-based fluorescent probes recently reported by Yin *et al*. [121](#page-123-5) Our group also reported a dual emission fluorescent probe, a rhodol thioester that detects GSH and  $Cys/Hey$  simultaneously.<sup>[122](#page-123-6)</sup>

62 We had an impressive achievement in developing a simple probe that can detect GSH levels both in plasma and in cells. This highly sensitive and selective probe is acrylate-based where the discrimination of GSH from structurally related analytes is catalyzed by a cationic surfactant, cetyltrimethylammonium bromide (CTAB) micelle. The resorufin-acrylate indicator was successfully applied in deproteinized human blood plasma and will be described in detail in section  $5.3$ .<sup>[123](#page-124-0)[,124](#page-124-1)</sup> Prior to that, Strongin's group had designed a seminaphthofluorescein (SNF) acrylate-based probe (**43**) which detected Cys selectively over GSH and Hcy.<sup>[125](#page-124-2)</sup> The sensing mechanism was based on a tandem conjugate addition of **43** to the thiol group followed by an intramolecular cyclization reaction to release the free SNF fluorescent dye (Figure 5.2). The conjugate addition reaction to form thio-ethers is non-selective; however, the second step (intramolecular cyclization) differs among the three thiols due to different kinetics. The intramolecular cyclization reaction to form a 7-membered ring for Cys is kinetically favored over the formation of 8- and 12-membered rings in the case of Hcy and GSH respectively. Thus Cys selectivity was based on different relative rates of intramolecular cyclization.



Figure 5.2 Proposed mechanism for discrimination of Cys from Hcy using probe **45**. [125](#page-124-2)

To achieve selective detection of GSH over Cys and Hcy, one would need to overcome the formidable challenge of favoring the formation of a larger ring (12 membered for GSH) over a 7- and 8-membered ring in the case of Cys and Hcy respectively. Wei and co-workers reported that cetyl-trimethyl-ammonium bromide (CTAB, **46**) micelles can catalyze the intramolecular ring closure of larger rings, reversing the expected kinetics based on ring size.<sup>[126](#page-124-3)</sup> In their study, they measured the rates of cyclization of an intramolecular Williamson ether reaction (Figure 5.3) for the formation of 7- to 20-membered rings and observed a 500-1500-fold decrease in ring closure on going from a 7-membered ring to a 14-membered ring in homogeneous environments (99% DMSO, 75% EtOH) and only a 6-fold decrease in the micellelocalized reaction.



cetyl-trimethyl-ammonium bromide (CTAB) 46



Figure 5.3 Intramolecular Williamson ether reaction.<sup>[126](#page-124-3)</sup>

In another study, it was reported that GSH binds the positively charged surface of CTAB micelle through some electrostatic interactions between the carboxylate groups and the cationic CTAB surface.<sup>[127](#page-124-4)</sup> Based on this, we envisioned that a relatively smaller, flat and more planar dye similar to  $PhSeO<sub>2</sub>H$  (Figure 5.4) should fit well within the micelle allowing a good self-assembly of CTAB micelle with the probe through hydrophobic and electrostatic interactions in water bringing it in close proximity to GSH.

We then proceeded to design a very simple resorufin-acrylate based probe that successfully detected GSH in human plasma.



Figure 5.4 Proposed Model for Selenium-Mediated Micellar.<sup>[127](#page-124-4)</sup>

\*Adapted with permission from *Langmuir*, 2007, Volume 23, pages 1518-1522; Huang, X.; Dong, Z.; Liu, J.; Mao, S.; Xu, J.; Luo, G.; Shen, J. Selenium-Mediated Micellar Catalyst: An efficient Enzyme Model for Glutathione Peroxidase-like Catalysis. Copyright 2007 American Chemical Society.

To rule out the possibility of detecting GSH using acrylate-based probes which are large and 3-dimensional in shape in micelles, we designed a near-infrared (NIR) naphthofluorescein-based dye (**49**) and investigated its reaction selectivity in the presence of aminothiols. This probe was selective for Cys, thus eliminating any possibilities of achieving GSH selectivity with non-planar compounds. As predicted, the resorufin – acrylate probe (**50**) was successful in detecting GSH in deproteinized human plasma without any interference from related analytes such as Hcy and Cys. While developing asymmetric viologen probes specific for Hcy, to our surprise one of them,  $PhCV<sup>2+</sup>$  (24), detected GSH selectively without any interference from Hcy and Cys. This will be described in the next section.



Figure 5.5 Structures of acrylate-based probes

### **5.3 Results and discussion**

### 5.3.1 Acrylate-based probes

Probe **49** showed excellent selectivity towards Cys due to the reported kinetically favored formation of a 7-membered ring in the intramolecular cyclization step over the 8 and 12-membered rings for Hcy and GSH respectively. Upon reacting **49** with amino thiols, only the Cys containing sample developed a green color of the free dye whereas Hcy and GSH remained unchanged (Figure 5.6). Additionally, a significant absorbance response was observed for Cys and absolutely no response for related analytes. The concentrations of Cys and GSH used reflect their normal biological concentration in human plasma whereas the 15  $\mu$ M of Hcy was used to represent mild homocysteinemia. These findings indicate that this probe can serve as a selective "off-to-on" dosimeter for Cys with potential application in natural media. Moreover, the results confirmed our hypothesis that a relatively smaller, flat and more planar dye and not a large, 3 dimensional dye would fit well within the micelle allowing a good self-assembly of CTAB micelle with the probe for reaction with GSH.



Figure 5.6 CTAB-mediated response of **49** towards various aminothiols at pH 7.4. Absorption spectra of solutions of **49** (50 μM) in thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 7.4 (Phosphate buffer (50 mM). The inset shows the picture taken at 10 min.

67 To this end a resorufin acrylate probe (**50**) was developed and successfully applied in detecting GSH selectively via my coworkers using a CTAB micelle.<sup>[123](#page-124-0)</sup> Solutions of GSH, Cys and Hcy (2 equiv) with **50** in pH 7.4 phosphate buffer generated a characteristic strong pink color immediately upon addition of CTAB only in the presence of GSH (Figure 5.7a). Other amino acids, such as Hcy and Cys, did not exhibit significant changes under the same conditions. This interesting feature indicates that 4CTAB system can serve as a selective visual inspection dosimeter for GSH. Corresponding fluorescence increases were also observed (Figure 5.7b). Fluorescence upon reaction with GSH reached a plateau in less than 2 min.



Figure 5.7 Surfactant-mediated responses of solutions containing **50**-CTAB towards various thiols at pH 7.4. (a) Absorption spectra of **50** (2.5 μM) upon addition of thiols (2 equiv) in 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). The inset shows color changes of the solution of 4 (10  $\mu$ M) upon addition of thiols (2 equiv) in 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). The picture was taken immediately upon addition of CTAB; (b) Fluorescence spectra (λex = 565 nm) of **50** (2.5 μM) upon addition of thiols (2 equiv) in 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra were taken immediately upon addition of CTAB. The inset shows time-dependent fluorescence changes ( $\lambda$ em = 587 nm) of the same system.

Based on the above results, we proposed a plausible mechanism for the GSH selectivity of the probe-CTAB system that involves the conjugate addition of GSH to **50** to generate **51**, which in turn undergoes an intramolecular cyclization/elimination reaction sequence catalyzed by the CTAB micelle releasing the free resorufin dye (Figure 5.8), resulting in the recovery of the fluorescence. Formation of the 12-membered ring (**52**) and the free resorufin dye (**53**) were confirmed by HRMS.



Figure 5.8. Proposed mechanism for the selective detection of GSH in CTAB medium that involves a conjugate addition reaction followed by a micelle-promoted 12-membered ring formation/elimination sequence. <sup>[123](#page-124-0)</sup>

# 5.3.2 Improved resorufin-acrylate selectivity towards  $GSH<sup>124</sup>$  $GSH<sup>124</sup>$  $GSH<sup>124</sup>$

While the probe-CTAB-GSH signal is high at pH 7.4, it is known that acrylate esters are susceptible to hydrolysis at high pH and that GSH is also relatively unstable under the same conditions (half-life of 9 hours at pH 7.4 compared to 16 hours at pH  $6.5$ .<sup>[128](#page-124-5)</sup> Chemical stability of fluorogenic probes is very important because spontaneous hydrolysis raises background fluorescence and compromises the ability to assess its reactivity with analytes. To address the challenge of probe hydrolysis, my own work involved investigating and optimizing the effect of pH on the chemical stability of the probe.

The spectral behavior of the probe-CTAB system was examined over a wide range of pH values (pH 5.5 to pH 8) and its response to the various thiols was studied at lower pH values. As expected, the acrylate-based probe **50** showed the greatest background signal at the higher pH values investigated. The probe-CTAB system was most stable at lower pH values (Figure 5.9).



Figure 5.9 Spectral behavior of the probe-CTAB system under different pH conditions (50 mM phosphate buffer). Time-dependent absorbance changes of a solution of **50** (2.5 µM) at 580 nm in CTAB media (2 mM) buffered at pH 5.5 to 8.

We investigated the response of **50** towards amino thiols at pH 6 and observed that the reaction is less rapid as compared to pH 7.4 (Figure 5.10) and the selectivity towards GSH was further enhanced through the complete elimination of any residual Cys and Hcy response (Figure 5.11). Very little background interference from the hydrolysis of the probe is observed starting at 10 min after mixing. Thus, pH 6 was chosen for further application studies in plasma.



Figure 5.10 Surfactant mediated response of the probe-CTAB system towards various thiols (5 μM) at pH 6.0. Time-dependent absorbance changes of a solution of **50** (2.5 µM) at 583 nm in CTAB media (2 mM) buffered at pH 6 (phosphate buffer, 50 mM).



Figure 5.11 Absorption spectra of **50** (2.5 μM) upon addition of thiols (2 equiv) in 2.0 mM CTAB media buffered at pH 6 (phosphate buffer, 50 mM) at 8 min.

To evaluate the applicability of the probe-CTAB system in complex natural media, fluorescence determination was performed in 10% deproteinized human plasma. Plasma proteins were precipitated using MeCN (two thirds of the reconstitution volume) and removed by centrifugation at 4,000 rpm for 30 min. The supernatant liquid was diluted and added to a solution of **50** (1 μM) in phosphate buffer (pH 6, 50 mM) in the presence of 2.0 mM CTAB. The fluorescence response of replicate  $(n = 3)$  samples and GSH spiked samples were monitored as above and the GSH content in the plasma sample was determined from the regression equation of a standard calibration curve (Figure 5.12) (a) and (b)). The GSH content of the plasma sample was determined to be  $3.24 \pm 0.14$ μM, which is well within the reported GSH concentration range for human plasma samples from healthy individuals. <sup>[129](#page-124-6)</sup>



Figure 5.12. Determination of GSH in human plasma using the probe-CTAB system. (a) Calibration curve of **50** (1.0 μM) in 2.0 mM CTAB media buffered at pH 6 (phosphate buffer, 50 mM) showing a linear relationship between fluorescence intensity ( $\lambda$ ex = 565 nm,  $\lambda$ em = 587 nm) and GSH concentration (0.1– 1.2 μM); (b) Fluorescence spectra ( $\lambda$ ex = 565 nm) of **50** (1.0 μM) upon addition of GSH (0–1.0 μM) to 10% deproteinized plasma diluted with 2.0 mM CTAB media buffered at pH 6.0 (phosphate buffer, 50 mM). The calibration curve and emission spectra were collected 8 min after mixing.

Accuracy assessment of the method was conducted using recovery experiments.<sup>[130](#page-124-7)</sup> Recoveries of the known spiked amounts of GSH were between 99.2% and 102.3% with a generally satisfactory precision (Table 5.1). These results revealed the potential applicability and reliability of using **50** in quantitative detection of GSH in human plasma.

Sample	<b>GSH</b> Spiked	<b>GSH Measured</b>	Recovery	<b>RSD</b>
	$(\mu M)$	(µM)	$\mathcal{O}_0$ )	$(\%)$
10% Plasma		0.324	$\overline{\phantom{0}}$	4.42
$10\%$ Plasma + GSH	0.3	0.631	102.3	4.90
$10\%$ Plasma + GSH	0.6	0.919	99.2	4.24
$10\%$ Plasma + GSH	0.9	1.224	100.0	5.88

Table 5.1. Determination of GSH content in 10% deproteinized human plasma samples.

### 5.3.3 Asymmetric viologen-based probe

The response of PhCV<sup>2+</sup> (24) towards various aminothiols was examined at pH 9 (Tris buffer, 0.5 M). Initial investigation of **24** at a concentration of 1 mM in thiols solutions (1 mM) showed no selectivity. The reaction was optimized by lowering probe/thiols concentration and surprisingly at 500 μM probe concentration and 500 μM, a useful absorption response was observed in the presence of GSH (Figure A8, Appendix A). A minimal response was promoted by the presence of Hcy and Cys. Further optimization via lowering the thiol concentration to 250 μM resulted in the complete elimination of residual responses from Hcy and Cys, thereby affording excellent GSH selectivity (Figure 5.13). Attempts to lower thiol concentration to physiological levels (15 μM Hcy, 250 μM Cys and 6 μM GSH) led to loss of selectivity. Hence, this probe cannot be applied to determine GSH at relevant plasma levels. However, the probe is potentially of high utility for detecting GSH in blood where levels are higher  $(1-2 \text{ mM})$  $(1-2 \text{ mM})$  $(1-2 \text{ mM})$ .<sup>1[,4](#page-107-3)</sup>



Figure 5.13 Spectral response of PhCV<sup>2+</sup> (24) towards various amino thiols at pH 9. Absorption spectra of solutions of PhCV<sup>2+</sup> (500 μM) in thiol solutions (250 μM) buffered at pH 9 (Tris buffer (200 mM). The inset shows the picture taken at 25 min.

Concentration-dependent studies were performed, and absorbance changes at 510 nm were found to be linearly proportional to the concentrations of GSH (0–500 μM). This suggested a potential application towards quantitative determination of GSH (Figure 5.14).



Figure 5.14. Absorption spectral changes of **24** upon addition of increasing concentrations of GSH (0-500 μM). Inset: absorbance changes at 510 nm as a function of the concentrations of GSH. All solutions were composed of 200 mM Tris buffer (pH 9) and **24** (500 μM).

To investigate the possible involvement of free radicals, EPR studies of the probe were carried out in the absence and presence of GSH. Interestingly, **24** alone produced an EPR signal of greater amplitude compared to the one generated in the presence of GSH (Figure 5.15). Thus, the presence of GSH diminished the amount of radical species that were generated by the probe itself. Although this experiment suggested the possibility of a free radical mechanism being involved, after samples were taken out from the EPR instrument, we observed precipitation, an indication that the data may not reflect the mechanism. Further investigations were performed including mass spectrometry. NMR studies were not possible because of solubility issues of the probe at higher concentrations needed.



Figure 5.15 EPR spectrum of  $PhCV^{2+}$  (24), (20 mM) in the presence and absence of GSH (10 mM) at pH 9 (200 mM, Phosphate buffer).

Since Hcy selectivity would be more favorable if all thiols are forming the reducing, α-amino carbon-centered radical, we propose that there are other factors enabling selectivity for GSH. These include favorable structural and/or electrostatic interactions between the probe (cationic) and anionic GSH. These also could promote supramolecular assembly formation.<sup>[131](#page-125-0)</sup>

Molecular calculations (MM2, Gasteiger-Hückel charges) using the SYBYL-X™ (version 2.0, Certara, L.P.) suite reveal that the interactions of **24** with GSH are in fact, driven by electrostatics and the spatial configuration of **24** is dramatically modified as a result (Figure 5.16).



Figure 5.16. Energy minimized structures of **24** (left) and **24** in the presence of GSH (right).

### **5.4 Experimental section**

## 5.4.1 Materials and instruments

All chemicals were purchased from Sigma-Aldrich or Acros and used without further purification.<sup>1</sup>H-NMR and <sup>13</sup>C-NMR spectra were recorded on a Bruker AMX-400 NMR spectrometer, using TMS as an internal standard. ESI-HRMS (high resolution mass spectrometry) spectra were obtained on a Thermo Electron LTQ Orbitrap hybrid mass spectrometer. UV-visible spectra were collected on a Cary 50 UV-Vis spectrophotometer; Fluorescence spectra were collected on a Cary Eclipse (Varian, Inc.) fluorescence spectrophotometer with slit widths set at 5 nm for both excitation and emission, respectively. The high voltage of the fluorescence spectrophotometer was set at 550 V and pH measurements were carried out with an Orion 410A pH meter.

## **5.4.2 Synthesis of the NIR acrylate 49**



Figure 5.17 Synthesis of NIR acrylate probe **51**

# **Improved synthesis of 1, 13-dihydroxy-3' H-spiro[dibenzo[c,h]xanthene-7,1' isobenzofuran]-3'-one, 56**

This compound was previously synthesized by our group  $132$  in 18% yield and here we modified the procedure by allowing the reaction to run for a longer time, 24 h compared to the previously used 16 h. Additionally, commercially available **54** was used instead of synthesizing it. This resulted in a pure compound in high yield and didn't require purification by flash chromatography as before. 1,8-dihydroxy naphthalene, **54** (0.5 g, 3.12 mmol), and phthalic anhydride **57** (0.231 g, 1.56 mmol) are dissolved in 2 mL of methanesulfonic acid. To this solution is added 2 mL of TFA the mixture is heated

and stirred at 80 °C for 24 h. The reaction mixture is cooled to room temperature and then poured into 100 mL of DI water. The precipitated solid is filtered and washed with DI water ( $5 \times 100$  mL) to give a pure grey compound which is air-dried overnight. Yield 0.958 g, 71%. <sup>1</sup>H NMR (400 MHz, DMSO) δ 11.34 (s, 2H), 8.14 – 8.09 (m, 1H), 7.82-7.75 (m, 2H), 7.62 (d, *J* = 8.8 Hz, 2H), 7.53 (t, *J* = 7.8 Hz, 2H), 7.44 (d, *J* = 7.5 Hz, 2H), 7.39 (d, *J* = 6.8 Hz, 1H), 7.12 (d, *J* = 6.9 Hz, 2H), 6.75 (d, *J* = 8.7 Hz, 2H).

## **1-hydroxy-3'-oxo-3'H-spiro[dibenzo[c,h]xanthene-7,1'-isobenzofuran]-13-yl acrylate, 51**

Under argon compound **51** (0.200g, 0.463mmol) and Et<sub>3</sub>N (0.129 mL, 0.925) mmol) are dissolved in 15 mL anhydrous DCM, then acryloyl chloride (0.094 mL, 1.16 mmol) in 5 mL DCM is added dropwise at  $0^{\circ}$ C. The reaction mixture is stirred at this temperature for 1 h, then warmed to rt and stirred overnight. The resulting mixture is diluted with DCM (20 mL), washed with water (20 mL  $\times$ 3) and dried over anhydrous Na2SO4. The solvent is removed in *vacuo* and the target compound is isolated by flash column chromatography on silica gel using  $CH_2Cl_2$ : MeOH 98:2 for elution to yield a cream powder 0.128g, 57%. <sup>1</sup>H NMR (400 MHz, CDCl3)  $\delta$  9.41 (s, 1H), 8.12 – 8.07 (m, 1H), 7.80 (d, *J* = 7.5 Hz, 1H), 7.68 – 7.59 (m, 4H), 7.53 – 7.47 (m, 2H), 7.40 – 7.33 (m, 2H), 7.18 – 7.12 (m, 2H), 7.00 – 6.91 (m, 2H), 6.79 (d, *J* = 8.7 Hz, 1H), 6.60 (dd, *J* = 17.3, 1.3 Hz, 1H), 6.01 (dd,  $J = 10.4$ , 1.3 Hz, 1H). <sup>13</sup>C NMR (101 MHz, CDCl3)  $\delta$ 169.40, 165.43, 153.80, 153.28, 147.12, 145.58, 145.19, 136.57, 135.44, 134.25, 130.12, 129.15, 127.15, 127.06, 125.80, 125.56, 124.23, 124.08, 123.26, 122.03, 119.59, 117.84,

79

114.51, 113.39, 112.93, 112.50, 82.08. HR ESI  $[M+H]^+$ ,  $m/z$ : 487.1182 calc for  $C_{31}H_{19}O_6^+$  487.1186.

5.4.3 CTAB-mediated spectral responses of acrylate probes towards thiols general procedure.

The acrylate probe is added to solutions of thiols in 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra (UV-Vis and Fluorescence) were collected immediately upon addition of the probe. In the case of deproteinized plasma, its proportion is 10% of the total volume after being mixed with the CTAB, buffer and probe solutions.

### **5.5. Conclusion**

Probe **52** can function as a simple new indicator for the highly selective and sensitive detection of GSH. This embodies a sensing mechanism that couples a conjugate addition reaction and a micelle-promoted 12-membered ring formation/elimination sequence. Due to the lack of fluorescence probes for the highly selective detection of GSH over other thiols in blood plasma, the discovery of **52** is highly significant. A new class of fluorescent probes for GSH may be developed through this new mechanism.

We have also developed a viologen probe **24** for selective detection of GSH without any interference from structurally related analytes via a binding interaction. This probe has potential for quantifying GSH as demonstrated by the linear relationship between **24** and GSH concentration.

## **CHAPTER.6: TOWARDS DEVELOPING A METHOD FOR DETECTION AND QUANTITATION OF GSH IN WHOLE BLOOD DEPOSITED ON FILTER PAPER**

### **6.1 Introduction**

There is often not a clear correlation between whole blood GSH and plasma GSH levels. This has been seen for example in the initial phase of sepsis where plasma concentrations of GSH decreased, whereas GSH status in skeletal muscle and whole blood remain unaltered.<sup>[133](#page-125-2)</sup> In contrast, in another recent study investigating temporal changes in whole blood and plasma glutathione in hospital ICU patients with multiple organ failure, GSH levels from whole blood and not plasma were depleted in critically ill patients with chronic obstructive pulmonary disease.<sup>[134](#page-125-3)</sup> Levels of whole-blood glutathione in peritoneal dialysis patients have been used to monitor therapeutic outcomes.[135](#page-125-4) It is more efficient to use a whole blood GSH to diagnose mitochondrial disorders, as whole blood GSH levels are ca. 1000-fold higher than blood plasma levels.

Moreover, it has been noted that whole blood GSH measurements generally minimize variability caused by sample preparation steps.<sup>[136](#page-125-5)</sup> In general, whole blood GSH levels are indicative of the pathogenesis of major diseases that are often distinct from those that can be monitored using plasma GSH. Therefore, there is a need to develop simple methods that can detect and quantify GSH in whole blood.

The resorufin-acrylate probe though successful it has its own drawback that it's a short wavelength probe, hence its efficient function in a whole blood matrix would be hampered by optical interferences from hemoglobin (Hb). Several years ago, extreme sample dilution (e.g. 5000-fold) was used to minimize hemoglobin interference in the determination of GSH in dried blood spots on filter paper.<sup>[137](#page-125-6)</sup> Hb content would be reduced to less than 30  $\mu$ g/mL reducing absorbance near 415 nm to about 0.25 in a standard 1 cm cell. Dried blood specimens on filter paper are easy to obtain and work with and present much fewer logistical problems as compared to using plasma or whole blood samples. Only a small volume of blood is required. Disks are punched from the paper and the blood contents typically eluted/extracted into a small volume of solvent.

Apart from dilution, Hb can be removed using a commercial product, HemogloBind. This product can isolate and remove up to 90% of blood Hb.<sup>[138](#page-126-0)</sup> However, this still requires some dilution (500-fold dilution) and even with 10 % Hb remaining after HemogloBind processing, there is still Hb spectral overlap.

The work herein entails a new and relatively simple method for detection and quantitation of GSH in whole blood deposited on filter paper without interference from Hb.<sup>[124](#page-124-1)</sup> The method involves deproteinization of blood extracted from a filter paper with concomitant fractionation of GSH using size exclusion chromatography (Figure 6.1). In the process Hb would be completely removed from the fraction containing GSH. This would be an ideal method for drawing small sample volumes, which are easy to obtain from children and for enabling shipment of samples to a centralized lab. A small volume of blood dries quickly on paper as cells rupture, emptying their GSH stores. The method is also suitable in developing nations with limited access to refrigeration or electricity and in developed nations due to the rising healthcare costs and the high interest in hometesting kits.



Figure 6.1. A method for detection of GSH in whole blood deposited on a filter paper<sup>[124](#page-124-1)</sup>

Another advantage of this method is that deproteinization is carried out without using acids and organic solvents that can adversely affect biomolecules. Compared to the use of acids and organic solvents, filtration is a more benign method of removing proteins. The use of filters may also minimize the oxidation of GSH to GSSG.<sup>[139,](#page-126-1)[140](#page-126-2)</sup>

## **6.2 Results and discussion**

We successfully managed to show proof of concept that GSH can be fractionated away from proteins, Hb and other potentially interfering blood components very efficiently from a blood spot. Upon passing the extracted GSH from the dried blood spot (DBS) through the PD MiniTrap™ G-25 Sephadex column, all proteins elute in fractions 1, 2 and 3. This was confirmed by running UV-Vis absorption of the fractions and monitoring the peak at 290 nm (Figure 6.2). Only fractions 1, 2 and 3 exhibited significant absorption responses and none was observed in fractions 4 to 6. The other peaks at 400 nm, and 500-600 nm are a result of Hb which is highly absorbing. It can be observed that these peaks are absent in fractions 4, 5 and 6 suggesting that if GSH elutes in these fractions there wouldn't be any interference from Hb.



Figure 6.2. Absorption responses of DBS fractions in phosphate buffer at pH 7.4 Fractions were collected and immediately analyzed for absorption.

Fractions 4, 5 and 6 were then tested for the presence of GSH using the resorufinacrylate CTAB system. Upon addition of probe **50** (2.5 μM) to the fractions in 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer), significant fluorescence responses were observed in fractions 4 and 5 indicating the presence of native GSH in blood (Figure 6.3). The high responses in fractions 1, 2 and 3 are a result of the reaction of the probe with proteins. Fraction 6 behaved in the same manner as the blank.



Wavelength (nm)

Figure 6.3 Spectral response of **50** towards various DBS fractions at pH 7.4. Fluorescence spectra ( $\lambda$ ex = 565 nm) of **50** (2.5 μM) in solutions of DBS fractions and 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra were taken immediately upon addition of the probe.

To further confirm that fractions 4 and 5 indeed contained GSH, we examined commercial, standard GSH and collected all the six fractions. Upon addition of the probe and CTAB only fractions 4 and 5 developed a pink color as well as generating a significant fluorescence response as shown in figure A9 (Appendix A). Other fractions 1, 2 and 3 where proteins elute remained unchanged and their fluorescence responses were the same as the blank.

To investigate the effectiveness of this gel filtration method in deproteinizing dried blood, control experiments were performed using human serum albumin (HSA) at its whole blood concentrations (60 mg/mL). As expected no responses were observed in fractions 1, 2 and 3, confirming the absence of proteins in these fractions (Figure 6.4). This effectively means that the fluorescence responses observed in fractions 4 and 5 were due to native GSH and not residual proteins.



Figure.6.4 Absorption responses of HSA fractions in phosphate buffer at pH 7.4 Fractions were collected and immediately analyzed for absorption.

Another control experiment to rule out any interference from Hb was conducted using commercial Hb (20 g/dL). Hb was eluted together with proteins in fractions 1, 2 and 3 (Figure 6.5). No absorption response to Hb was seen in fractions 4, 5 and 6.



Figure 6.5 Absorption responses of Hb fractions in phosphate buffer at pH 7.4 Fractions were collected and immediately analyzed for absorption.

The same fractions were analyzed for their fluorescence response and as expected, upon addition of the probe and CTAB, no response was observed in fractions 4, 5 and 6 showing that this method completely eliminated all Hb (Figure 6.6). Any shorter wavelength probe that can selectively detect GSH in the absence of proteins and Hb can be applied with this method. We selected the resorufin-acrylate probe  $(50)$  over PhCV<sup>2+</sup> (**24**) due to its very low detection limit and its fast response.



Figure 6.6 Spectral response of **50** towards various Hb fractions at pH 7.4. Fluorescence spectra (λex = 565 nm) of **50** (2.5 μM) in solutions of DBS fractions and 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra were taken immediately upon addition of the probe.

We optimized our method to increase the GSH signal from the DBS by increasing the drying time from 3 hours to 24 hours (overnight). Interestingly, as shown in figure 6.7, the GSH signal increased significantly upon addition of the probe and CTAB. We also noticed the difference in the color of the filter papers spotted at these different times with the overnight filter paper looking completely dry. This was attributed to the complete rupture of the erythrocytes empting more GSH stores. For further studies, a drying time of 24 hours was used.



Figure 6.7 Spectral response of **50** towards various DBS fractions at pH 7.4. Fluorescence spectra (λex = 565 nm) of **50** (2.5 μM) in solutions of DBS fractions from blood dried at different times and 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra were taken immediately upon addition of the probe. (a) Blood dried for 3 h (b) Blood dried for 24 h.

Having identified the optimal conditions for GSH detection without any interference from proteins, Hb and other blood components, we investigated the potential of this method in quantifying GSH. The fluorescence response of **50**-CTAB system towards fractionated GSH increased linearly with incremental addition of GSH over a physiological relevant range (0-2 mM) (Figure 6.8 (a) and (b)). The concentration of GSH in a DBS of pig blood was determined to be 1.825 mM by standard addition which falls within the range of reported intracellular GSH levels (1-2 mM).



Figure 6.8 Spectral response of **50** towards DBS spiked with various concentrations of GSH. (a). Fluorescence spectra (λex = 565 nm) of **50** with increasing spiked GSH concentration (0-2 mM). (b) Calibration curve for **50** showing linearity between fluorescence intensity and spiked DBS with GSH. All solutions contained **50** (2.5 μM), 2.0 mM CTAB media and 50 mM phosphate buffer (pH 7.4).

During to the spotting and filtration process some GSH is lost. We evaluated this by comparing the fluorescence responses of standard GSH that underwent the entire process of spotting, extraction, reduction and filtration against one which didn't undergo the process. As shown in figure 6.9, more than 70% of native GSH from the DBS is recovered in this method, however the process can be optimized to reduce the losses.



Figure 6.9 Comparison of commercial GSH fractions vs non-fractionated GSH at pH 7.4. Fluorescence spectra (λex = 565 nm) of **50** (2.5 μM) in solutions of GSH fractions from commercial GSH (spotted, dried, extracted, reduced and separated by the column) and 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra were taken immediately upon addition of the probe.

### **6.3 Experimental section**

### 6.3.1 Fractionation of GSH

In this method blood is spotted on the filter paper and dried overnight, followed by extraction with buffer. Upon drying blood, cells are ruptured releasing GSH which in turn becomes oxidized to GSSG. Once oxidized, it is stable in dried blood specimens and can be assayed at a later time. In this assay the oxidized glutathione (GSSG) is reduced to GSH by treating it with the immobilized tris(2-carboxyethyl)phosphine (TCEP gel), a disulfide reducing agent. The reduced sample is passed through the PD MiniTrap<sup>TM</sup> G-25 Sephadex column where GSH is fractionated away from proteins, Hb and other potentially interfering blood components.

6.3.2 CTAB-mediated spectral responses of acrylate probes to GSH fractions.

The acrylate probe is added to fractionated solutions in 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra (UV-Vis and Fluorescence) were collected immediately upon addition of the probe.

## **6.4 Conclusion**

We have developed a new separation technique wherein glutathione can be fractionated away from proteins and other potentially interfering blood components very efficiently. This method eliminates the need to use very expensive materials like hemoglobind to remove Hb and allows for the use of shorter wavelengths probes to determine GSH in natural media. This assay has potential for quantitation of GSH in whole blood as demonstrated by the linear calibration curve.

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## APPENDIX A: SUPPORTING INFORMATION



Figure A1. Spectral response of  $MV^{2+}$  towards various spiked thiols in human blood plasma upon irradiation. Absorption spectra of solutions of  $MV^{2+}$  (50 mM) in human blood plasma and 0.5 M Tris buffer (pH 7.0) spiked with 1.5 μM Hcy, 25 μM Cys and 0.6 μM GSH. Plasma (10% v/v) was added to an argonsaturated solution of viologen, thiol and buffer and irradiated for 15 min using a Reptisun™ lamp.



Figure A2. Spectral response of  $BV^{2+}$  towards various spiked thiols in reduced human blood plasma upon irradiation. Absorption spectra of solutions of  $BV^{2+}$  (20 mM) in reduced human blood plasma and 0.5 M Tris buffer (pH 7.0) spiked with 1.5 μM Hcy, 25 μM Cys and 0.6 μM GSH. Plasma was incubated for 1 h with TCEP Gel and centrifuged at 1000 rpm for 5 min. The reduced, filtered plasma (10% v/v) was added to an argon-saturated solution of viologen, thiol and buffer and irradiated for 15 min using a Reptisun™ lamp.



Figure A3. Spectral response of  $BV^{2+}$  towards various spiked thiols in reduced human plasma upon irradiation. Absorption spectra of solutions of  $BV^{2+}$  (20 mM) in reduced human blood plasma and 0.5 M Tris buffer (pH 7.0) spiked with increasing concentrations of thiols. Plasma was incubated for 1 h with TCEP Gel followed by centrifugation at 1000 rpm for 5 min. The reduced plasma (10% v/v) was added to an argon-saturated solution of viologen, thiol and buffer and irradiated for 15 min using a Reptisun™ lamp.



Figure A.4 Spectral response of ACNV<sup>2+</sup> (26) towards various amino thiols at pH 8. Absorption spectra of solutions of ACNV<sup>2+</sup> (350 μM) in thiol solutions (15 μM Hcy, 250 μM Cys and 6 μM GSH) buffered at pH 8 (Phosphate buffer (80 mM) at 10 min.



Figure A.5 Cyclic voltammograms of current *vs* potential of asymmetric viologens and methyl viologen (4 mM) in phosphate buffer at 50 mV/s.



Figure A.6 Cyclic voltammograms of current *vs* potential of **24** and **25** (4 mM) in phosphate buffer at 100 mV/s.



Figure A.7 Cyclic voltammograms of current *vs* potential of **23** and **25** (4 mM) in phosphate buffer at 10 mV/s.



Figure A.8 Spectral response of  $PhCV<sup>2+</sup>$  (24) towards various amino thiols at pH 9. Absorption spectra of solutions of PhCV<sup>2+</sup> (500 μM) in thiol solutions (500 μM) buffered at pH 9 (Tris buffer (200 mM).



Figure A9 Spectral response of **50** towards various commercial GSH fractions at pH 7.4. Fluorescence spectra (λex = 565 nm) of **50** (2.5 μM) in solutions of GSH fractions and 2.0 mM CTAB media buffered at pH 7.4 (phosphate buffer, 50 mM). Spectra were taken immediately upon addition of the probe.








































