

# A Computer Model of Intracranial Pressure Dynamics during Traumatic Brain Injury that Explicitly Models Fluid Flows and Volumes

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# Objective

- To create a computer model of intracranial pressure (ICP) dynamics
- To use model to evaluate clinical treatment options for elevated ICP during traumatic brain injury (TBI)
  - Present work: replicate response to treatment
  - Future Work: predict response to treatment
  - Long term goal: optimize treatment

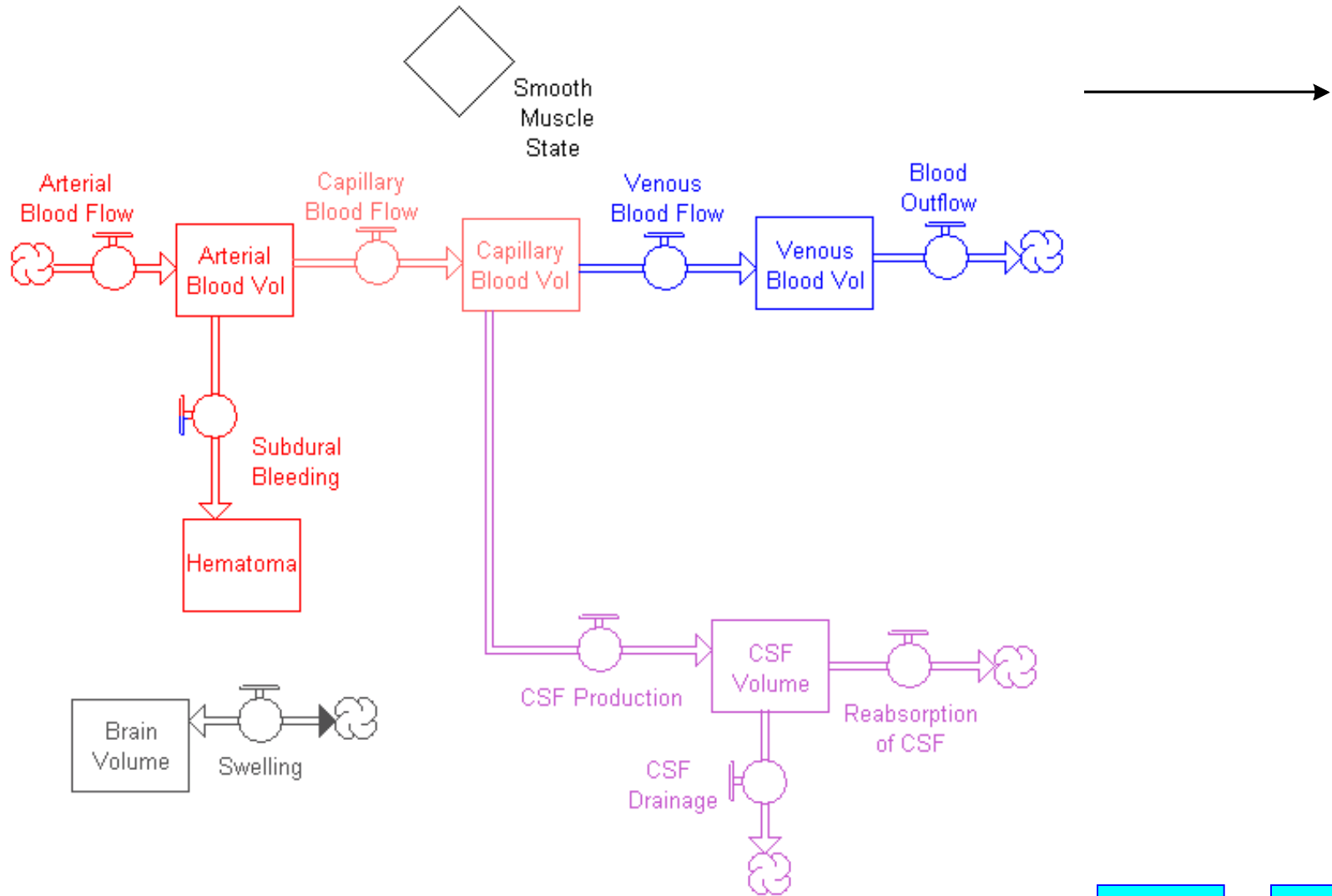
# Approach

- Fluid volumes as the primary state variables
  - Parameters estimated: compliances, resistances, hematoma volume and rate, etc.
  - Flows and pressures calculated from state vars. & parameters
  - Simplified logic used to model cerebrovascular autoregulation
    - ✓ Resistance at arterioles changes rapidly to adjust flow to match metabolic needs, within limits
    - ✓ The logic responds to diurnal variation or changes in ICP, respiration, arterial blood pressure, head of bed (HOB), etc.

# Approach (continued)

- **Trauma and therapies modeled**
  - Hemorrhage and edema
  - Cerebrospinal fluid drainage, HOB, respiration rate
- **Model calibrated to specific patients based on clinical data**
  - Recorded data includes ICP, ABP, and CVP
  - Data is clinically annotated
  - Data is prospectively collected per experimental protocol
    - ✓ Protocol includes CSF drainage, and changes in head of bead and minute ventilation
- **Tested capability of model to reproduce correct physiologic response to trauma and therapies**

# Model State Variables and Flows

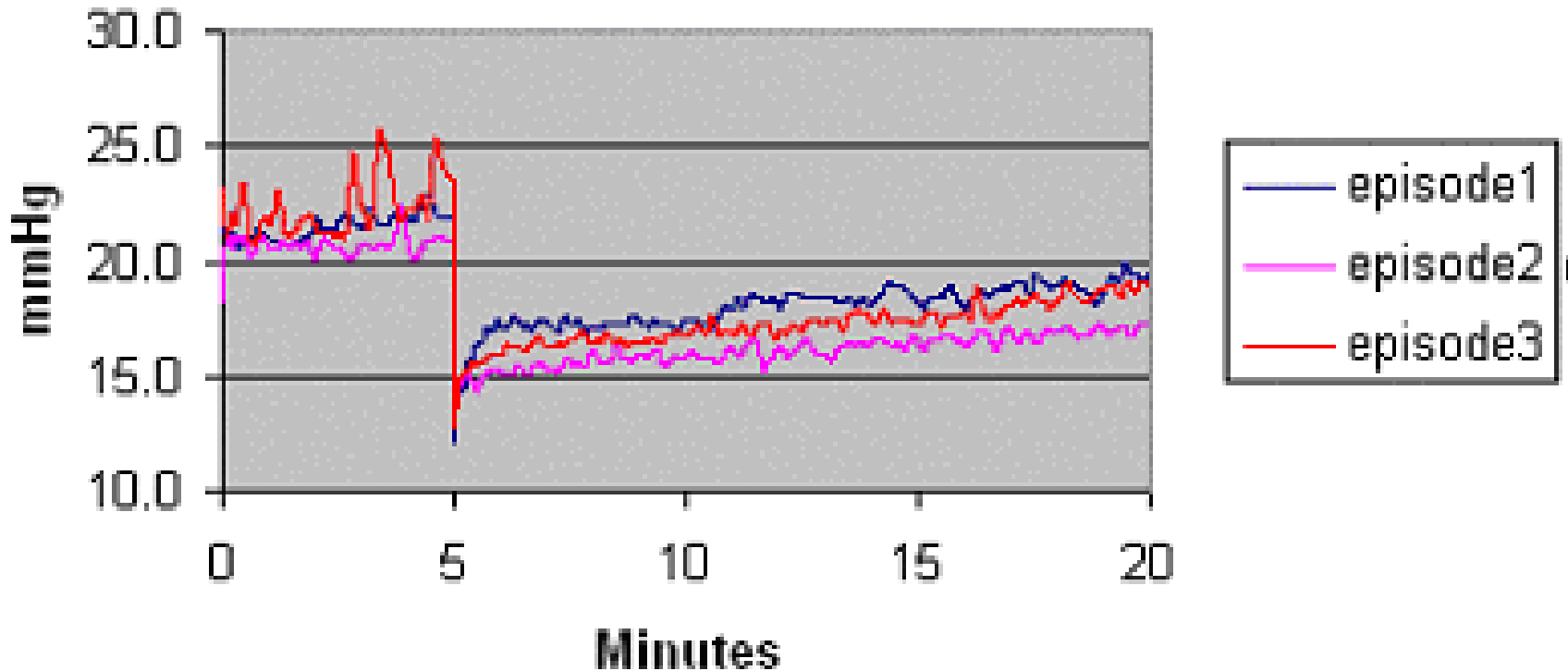


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[Full D.](#)

[Link to](#)  
[Eqns.](#)

# Clinical Data for ICP before and after CSF Drainage, Patient 1

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# Model Calibrated to Fit the Clinical Data for Patient 1

- Estimated parameters
  - *Initial hematoma volume* = 24 mL
  - *Hematoma increase rate* = 0
  - *CSF drainage volume* = 6.5 mL
  - *CSF uptake resistance* = 160 mmHg/mL/min
- ✓ This high value implies a significant impediment to flow/uptake
  - Presumably due either to the initial injury, subsequent swelling, or a combination of the two

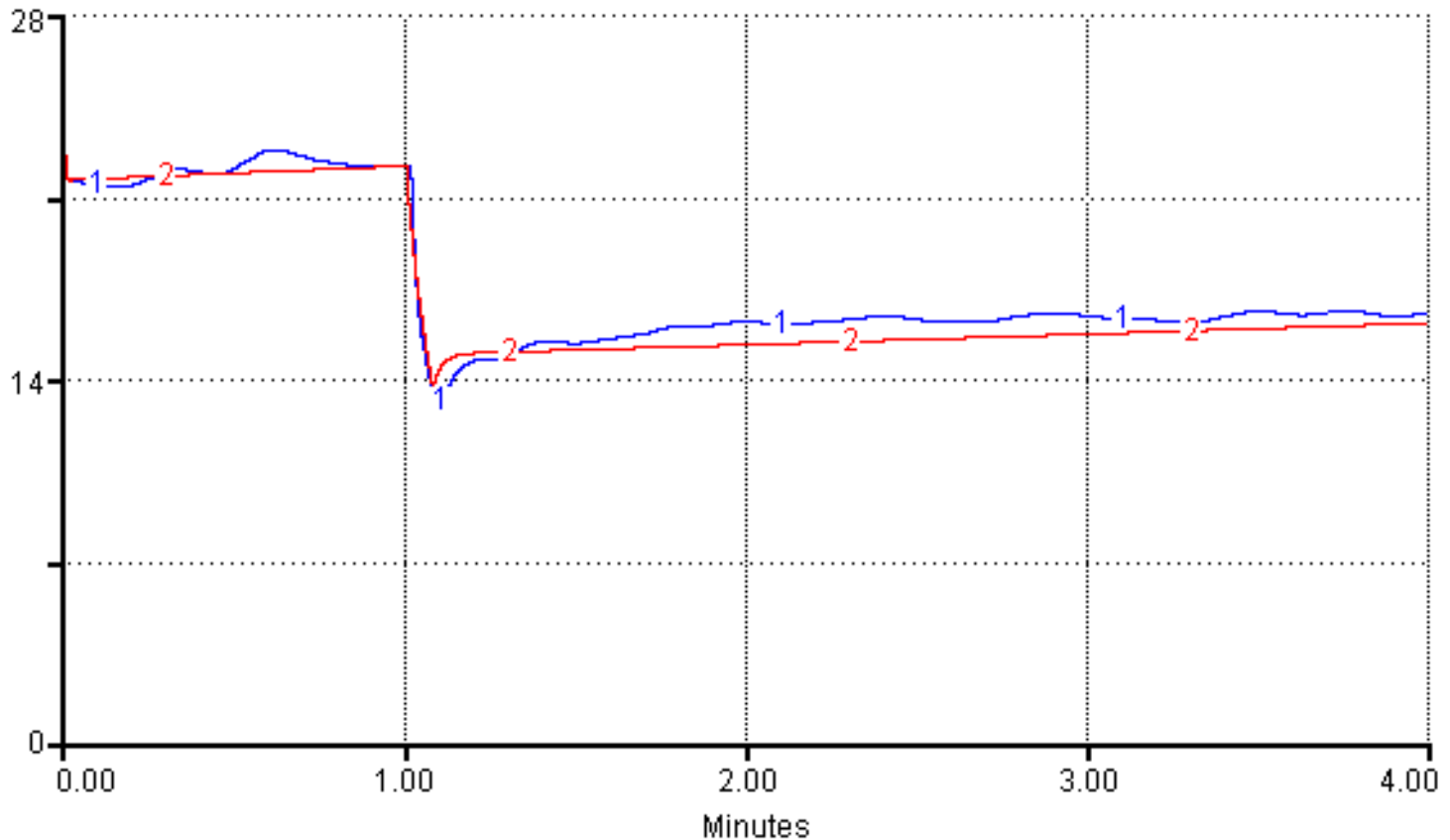
# Model Response to CSF Drainage, Patient 1

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ICP, Actual and Modeled (mmHg)

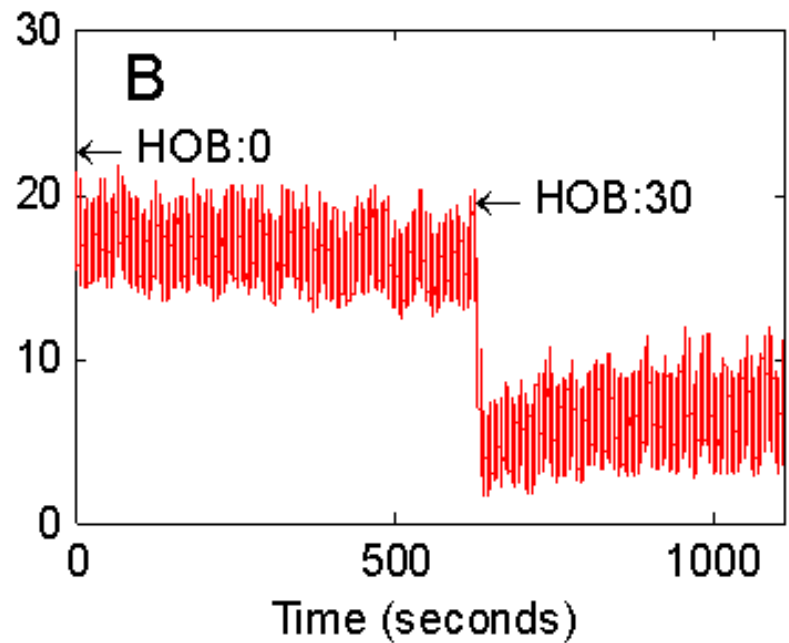
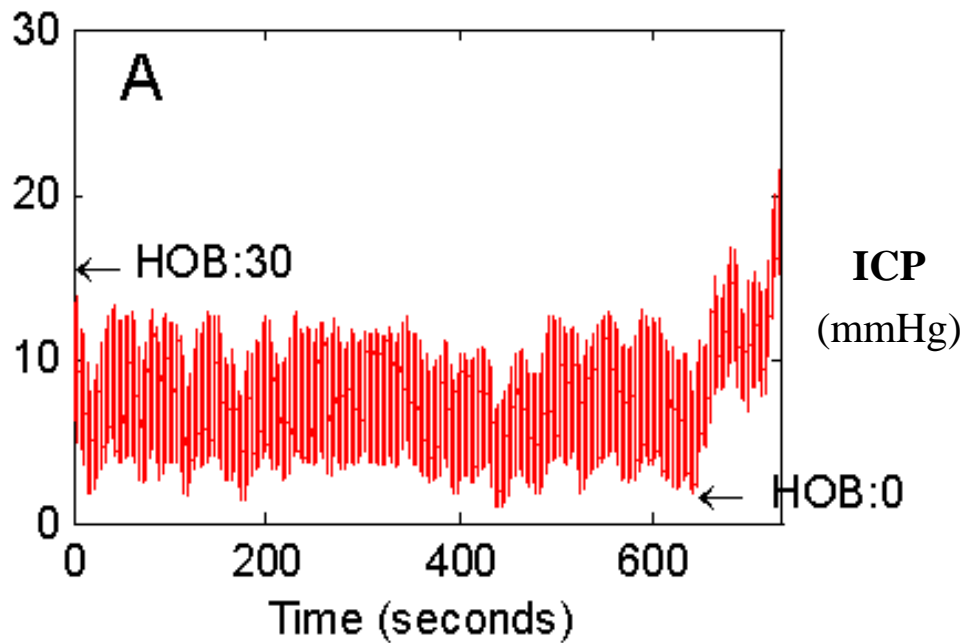
1: ICP Actual avg 3 episodes

2: ICP Modeled





# Prospective Clinical Data: Head of Bed Change, Patient 2



# Model Calibration for HOB Change, Patient 2

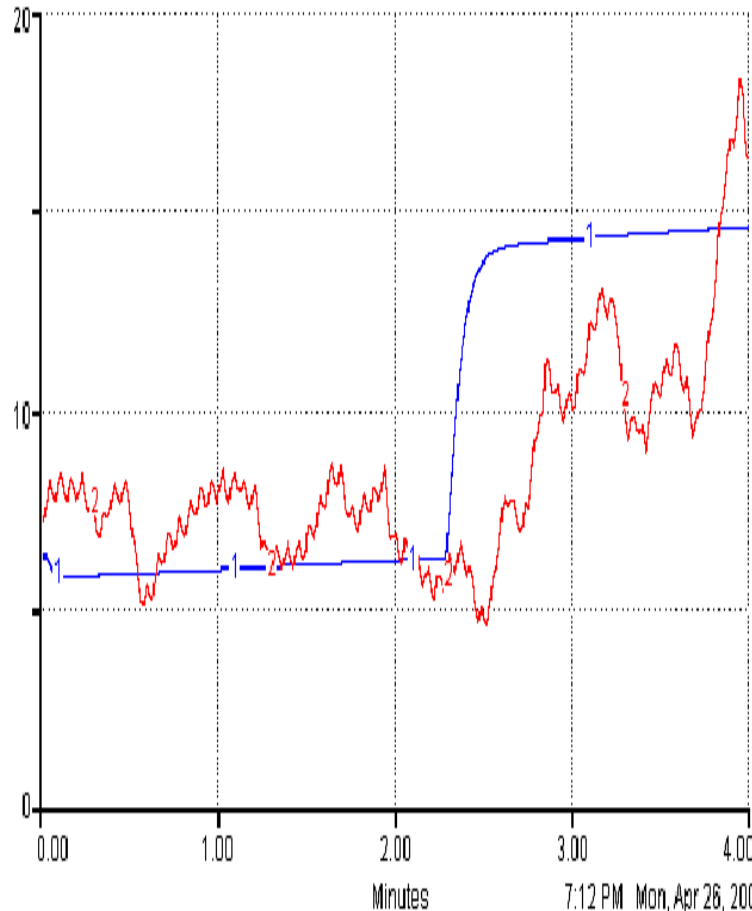
- Estimated parameters for lowering HOB
  - *Initial hematoma volume* = 6 mL
  - *Hematoma increase rate* = .5 mL/min.
  - *Distance from heart to brain* = 40 cm
  - *CSF absorption resistance* = 24 mmHg/mL/min
- Estimated parameters for raising HOB
  - *Hematoma increase rate* = .5 mL/min.
  - *Distance from heart to brain* = 45 cm (revised est.)

# Model Response to Changing HOB, Patient 2



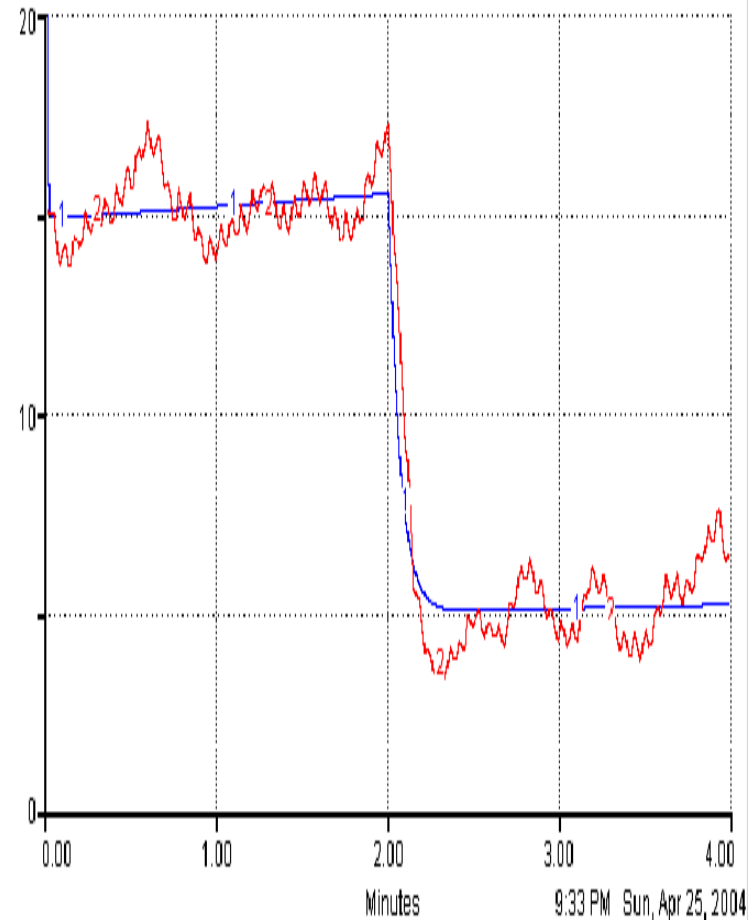
1: Modeled ICP

2: Actual ICP Episode A



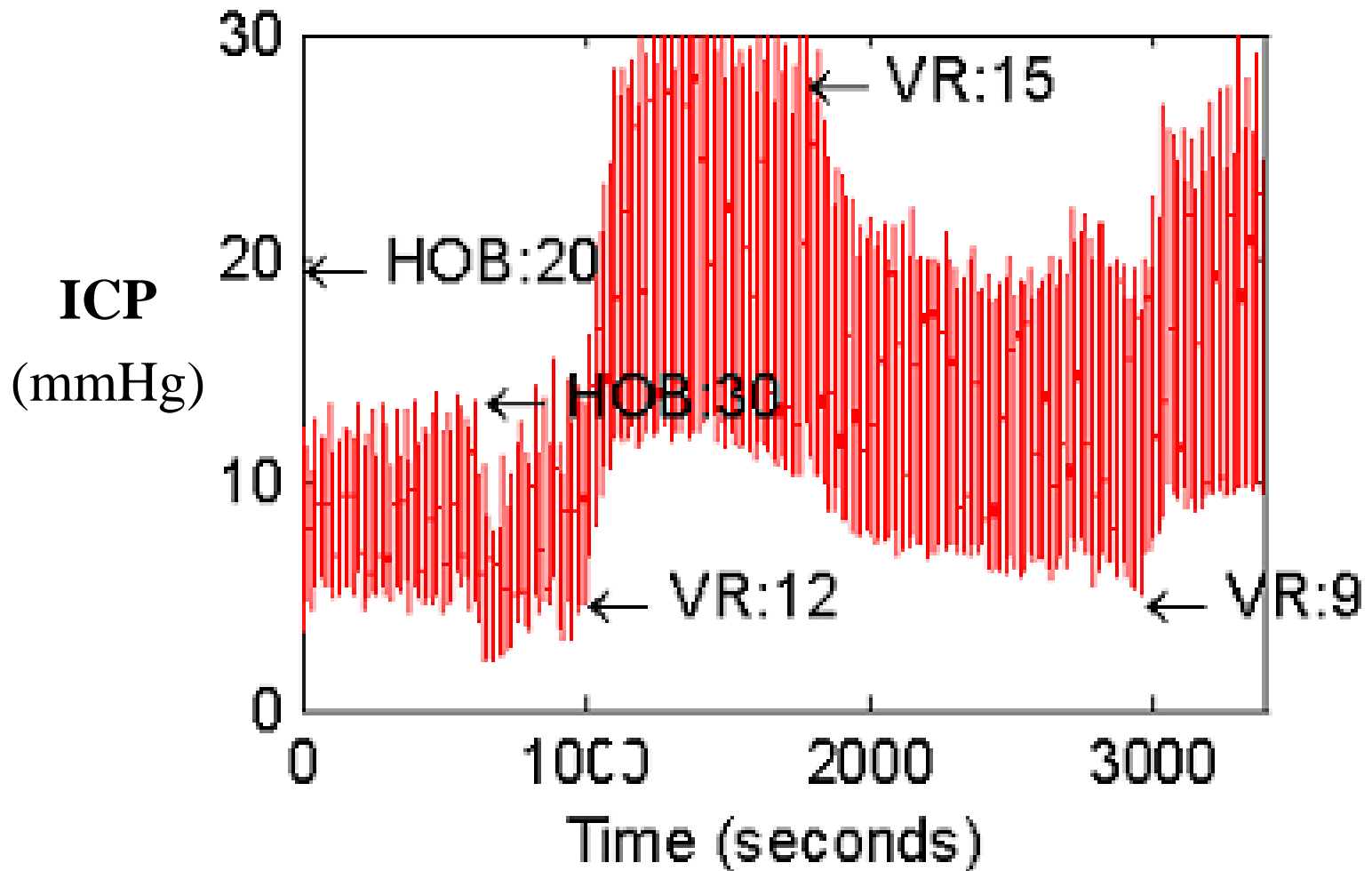
1: Modeled ICP

2: Actual ICP Episode B



# Prospective Clinical Data: Respiration Change, Patient 2

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# Model Calibration for Respiration Change

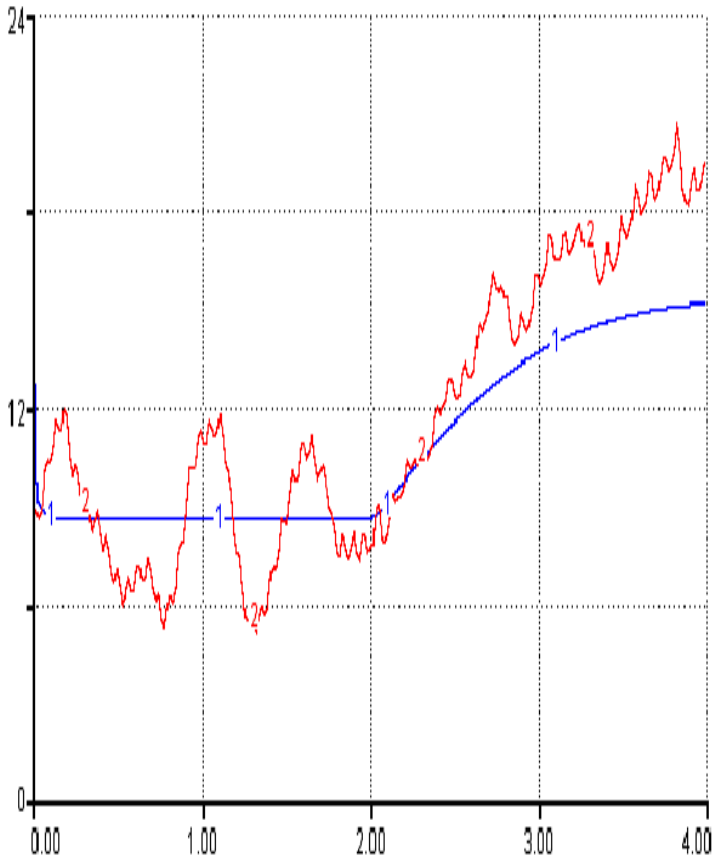
- Estimated Parameters for AR process
  - *Flow multiplier* = 75 ml/mmHg
  - *PaCO<sub>2</sub> setpoint* = 34 mmHg
  - *PaCO<sub>2</sub> offset* = 64 mmHg
  - *Conversion factor* = 2 mmHg-breaths/min.
  - *Time constant for PaCO<sub>2</sub> response* = 2.5 minutes
- The model was not able to fully replicate patient's response to the VR change
  - Most likely due to the simplified cerebrovascular autoregulation logic

# Model Response to Changing Respiration, Patient 2



1: Modeled ICP

2: Actual ICP Episode C1

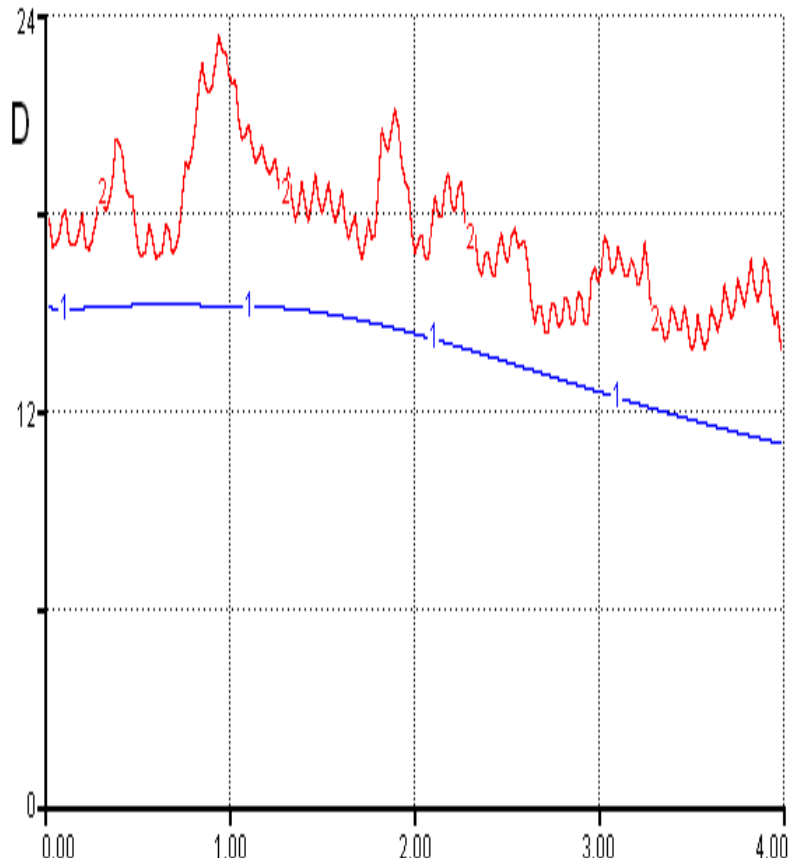


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1: Modeled ICP

2: Actual ICP Episode C2

Plot D



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# Summary

- We developed a simple model of ICP dynamics that uses fluid volumes as primary state variables
- ICP calculated by the model closely resembles ICP signals recorded during treatment and during an experimental protocol
  - CSF drainage, changing HOB and respiration
- Cerebrovascular autoregulation logic only partially captured the patient's response to respiration change

# Key Variables and Equations

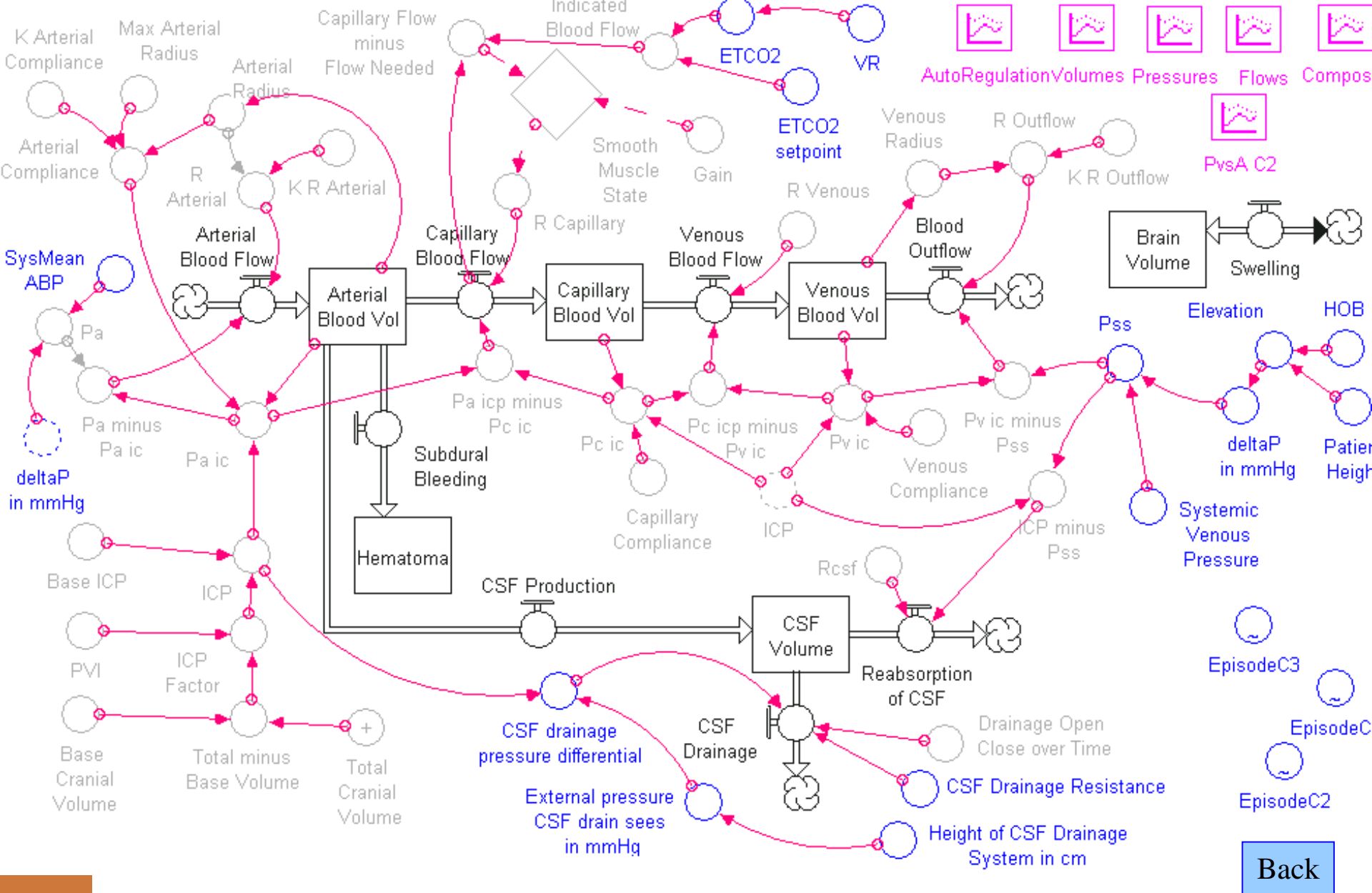
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- Six intracranial compartments
  - Arterial blood (ABV)
  - Capillary blood (CBV)
  - Venous blood (VBV)
  - Cerebral spinal fluid (CSF)
  - Brain tissue (BTV)
  - Hematoma (HV)
- Compartmental pressures
  - $P_{ab} = ICP + (ABV) / (\text{Arterial Compliance})$
  - $P_{cb} = ICP + (CBV) / (\text{Capillary Compliance})$
  - $P_{vb} = ICP + (VBV) / (\text{Venous Compliance})$
- Intracranial Pressure (ICP)
  - $ICP = \text{BaseICP} \times 10^{(\text{Total Cranial Volume} - \text{Base Cranial Volume}) / \text{PVI}}$

Back





# Hypothetical Test of the Model

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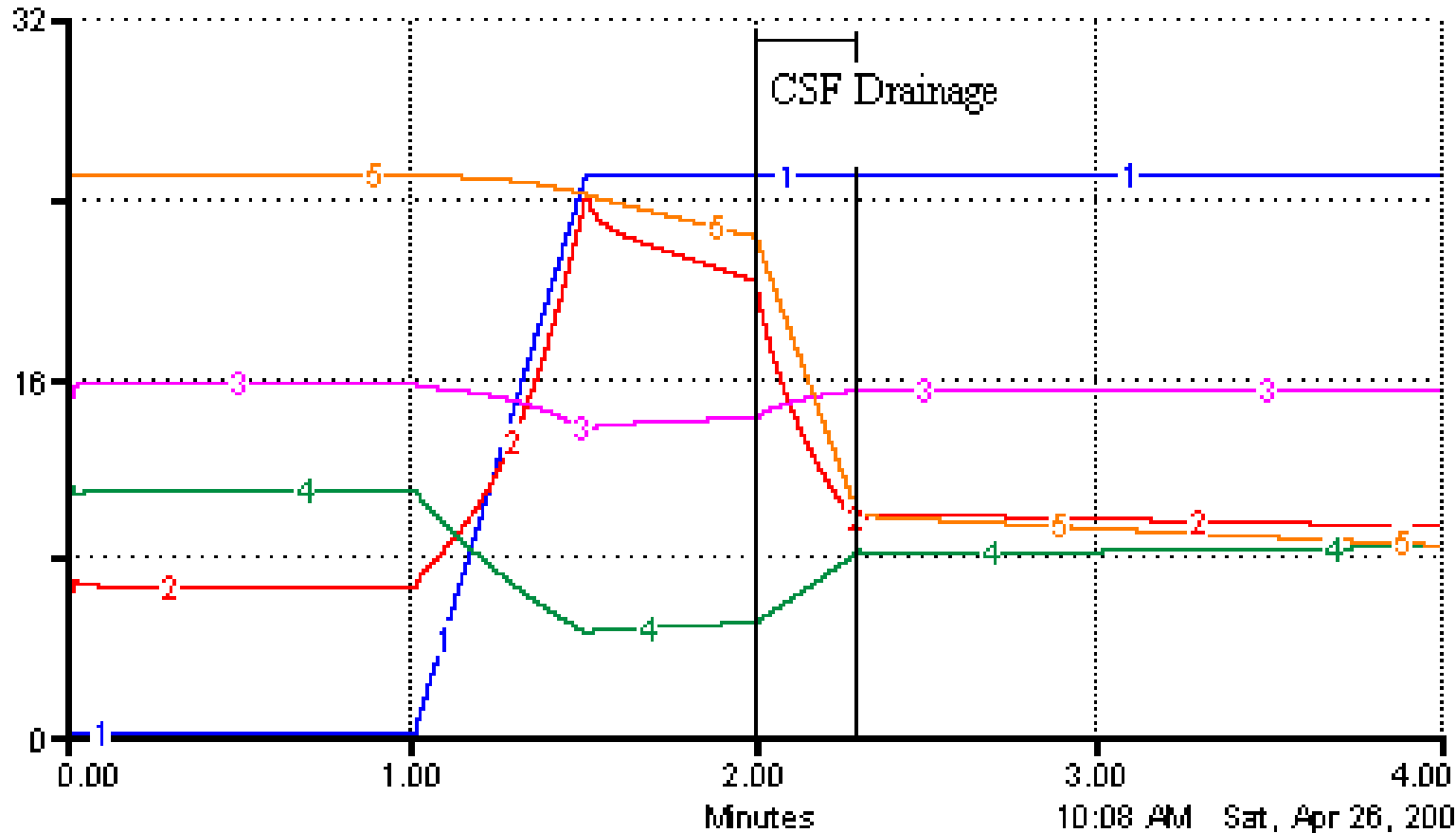
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	1.0-1.5 min.	2.0-2.3 min.
Perturbation	<ul style="list-style-type: none"><li>• Arterial blood escapes to form a 25 mL hematoma</li></ul>	<ul style="list-style-type: none"><li>• 12 mL Cerebral spinal fluid drained</li></ul>
Response	<ul style="list-style-type: none"><li>• ICP increases to 24 mmHg</li><li>• Venous and arterial blood is forced from the cranial vault</li></ul>	<ul style="list-style-type: none"><li>• ICP decreases to 10 mmHg</li><li>• Venous and arterial blood volumes normalize</li></ul>

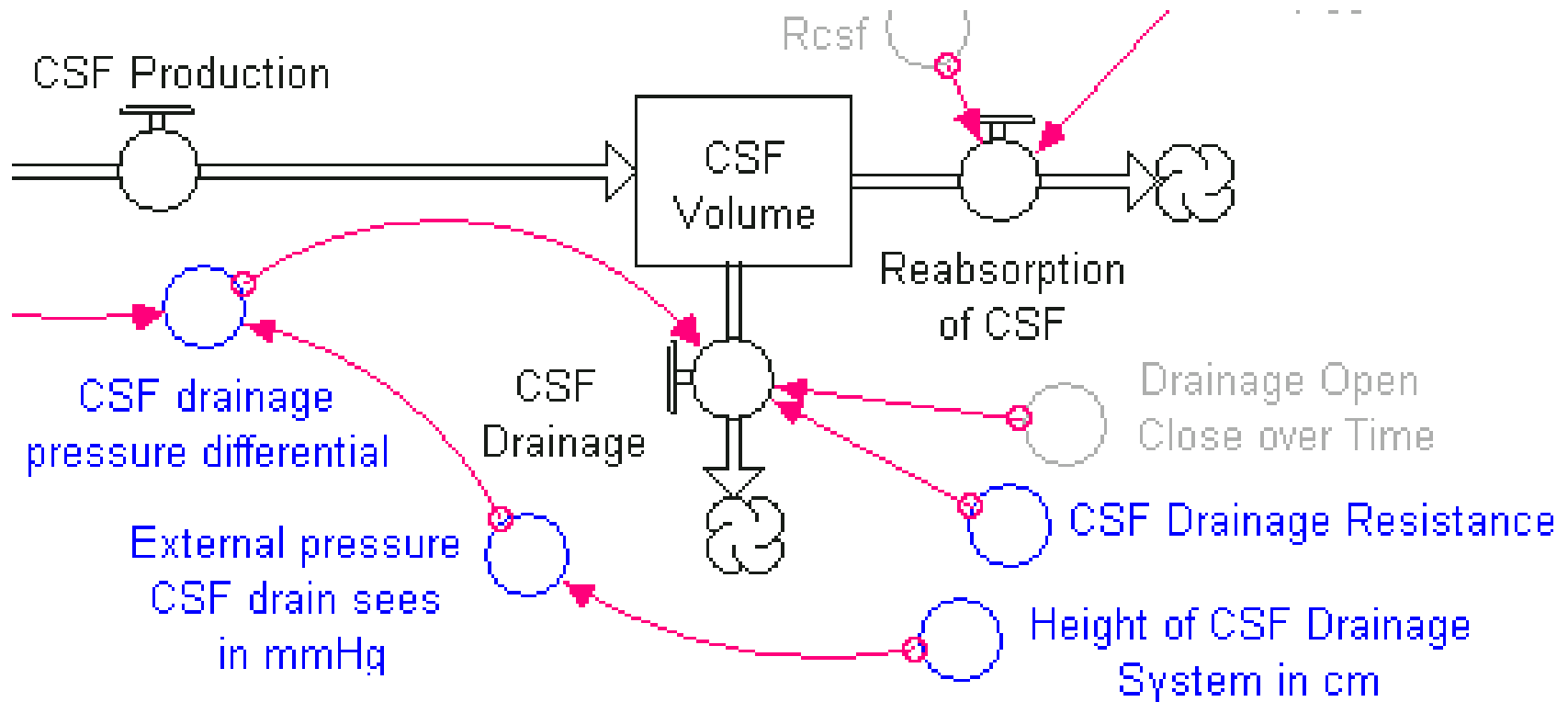
# Time Plot for Hypothetical Test of Model



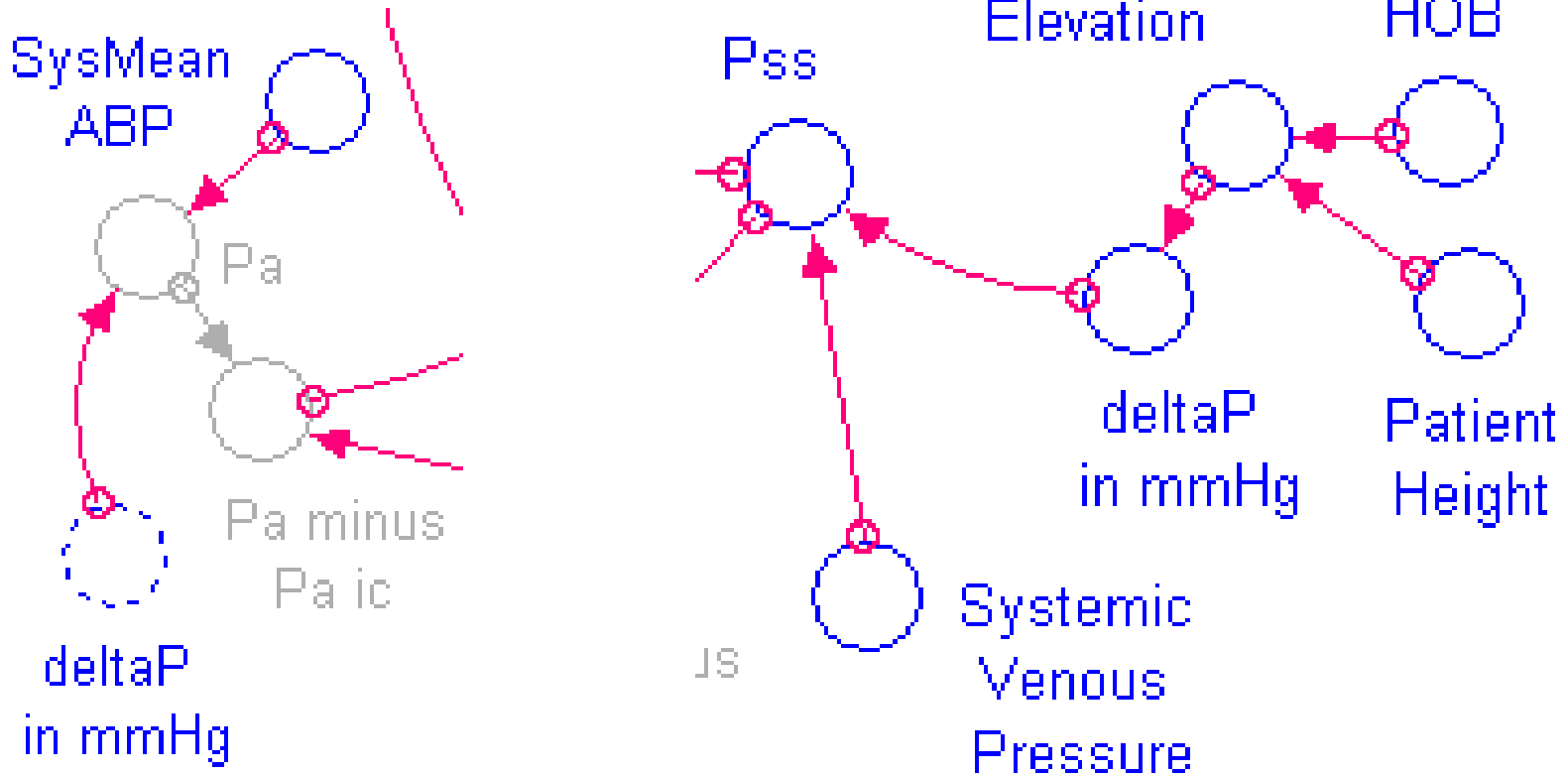
1: Hematoma      2: ICP      3: Arterial Blood Vol      4: Venous Blood Vol      5: CSF Volume



# CSF Drainage Submodel



# Head of Bed Logic



# Cerebrovascular Autoregulation (AR) Logic

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