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An Investigation of Tympanometric Measurements on an Older Adult Population

Marguerite Ann Fine

Portland State University

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Title: An Investigation of Tympanometric Measurements on an Older Adult Population.

APPROVED BY MEMBERS OF THE THESIS COMMITTEE:

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Robert Shotola, Ph.D.

Prior to this investigation, there appeared to be no published research data available on tympanometric configurations obtained from an older adult population. This study was designed to examine tympanograms obtained from an otologically normal, elderly population. Forty individuals, ranging in age from 59 to 83 years, participated in this study. All had a negative history of middle ear pathology and had normal tympanic membranes as determined by otologic examination. From
the eighty ears tested, fifty were used in this survey. Conductance and susceptance at 220 and 660 Hz were obtained at each ear and ranges for admittance were computed from these components. Additionally, acoustic reflex thresholds were obtained from this population.

The results obtained indicate that the values for the measures of conductance and susceptance are comparable to those from young adult groups. The reflex thresholds are slightly higher in the older group because their hearing thresholds are not as acute as those found in younger populations. Finally a larger percentage of the older population than might be expected was found to have evidence of healed perforations which were not discovered during otoscopic examination.

The present investigation demonstrated that additional normative data are needed in order that the otoadmittance meter be fully utilized with older adult populations.
AN INVESTIGATION OF TYMPANOMETRIC MEASUREMENTS
ON AN OLDER ADULT POPULATION

by

MARGUERITE ANN FINE

A thesis submitted in partial fulfillment of the requirements for the degree of

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in
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WITH EMPHASIS IN SPEECH PATHOLOGY AND AUDIOLOGY

Portland State University
1974
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David T. Clark, Dean of Graduate Studies and Research

November 25, 1974
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Finally, to my husband Wayne, my deepest thanks -- for his patience and his unfailing support and belief in me.
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CHAPTER I

INTRODUCTION

A relatively recent contribution to the field of audiometry has been the introduction of electroacoustic measuring instruments designed to evaluate middle ear functioning. This technique of measuring, recording, and evaluating changes in the tympanic membrane and middle ear cavity under conditions of varying air pressure has been termed tympanometry.

Prior to the introduction of the electroacoustic measurement instruments, it was difficult to determine the function of separate parts of the auditory system. With the electroacoustic bridge, the measurements can be restricted to a specific portion of the auditory system -- the middle ear. With this instrument, it has become possible to demonstrate acoustic manifestations of various pathological conditions in the middle ear, such as otosclerosis, otitis media, and ossicular discontinuities.

During the aging process, a certain amount of anatomical and physiological change takes place in the middle ear, involving the ligaments, muscles, and connective tissue. These changes, which are a result of the aging process, may cause a variety of lesions which are conductive in nature (Goodhill, 1969). There appears to be no published research data available on tympanometric configurations obtained from an elderly population. The establishment of tympanometric patterns common to the elderly should enhance the information now
available for clinical and research purposes.

Statement of Purpose

The purpose of the present study is to examine by the use of tympanometry, configurations obtained from an otologically normal, elderly population. Using the two probe tones of the Grason-Stadler Model 1720, the components of admittance -- conductance and susceptance -- will be investigated in order to gather data which may be used toward establishing working normative values. The information gathered will be compared with norms established for an otologically normal young adult population (Feldman, 1974; Jacobson, et al., 1973; Dirks and Morgan, 1973; and Porter, 1972), and the following question will be investigated: What are the differences, if any, between tympanograms obtained from a normal young adult sample and those obtained from a normal older adult sample.

It is hoped that the information obtained from this study will add to the diagnostic usefulness of tympanometry among older age groups.
CHAPTER II

REVIEW OF THE LITERATURE

The traditional approach to hearing assessment routinely includes the comparison of pure tone air-conduction thresholds with bone-conduction thresholds. The presence or absence of an air-bone gap yields information regarding the status of the middle ear, but gives little or no information regarding the cause of any conductive problems. In addition, audiometric tests rely primarily upon the patient's subjective decisions regarding the presence of the pure-tone stimuli. An otoscopic examination is limited to an inspection of eardrum mobility at extreme amplitudes of motion and gives inconclusive results in cases of conductive hearing loss, except those that are associated with gross changes in the anatomy, position, or mobility of the eardrum (Lamb and Norris, 1969; Zwislocki and Feldman, 1970).

The development of impedance measurements has provided a quantitative and objective measurement of middle ear functioning and has supplied a means of restricting these measurements to the middle ear only. It is now possible, through the use of impedance measurements, to detect middle ear pathologies that may not surface during otoscopic and audiometric examinations, and further, to differentiate among the various disorders (Metz, 1946; Zwislocki, 1957, 1961, 1963; Terkildsen and Nielsen, 1960; Lamb and Norris, 1969; and Zwislocki and Feldman, 1970).
Middle Ear Muscle System

In order to better understand the bases of impedance measurements, a knowledge of the functioning of the middle ear system is necessary. The tensor tympani and the stapedius, muscles in the middle ear, contract in response to sounds of loud intensity. The tensor tympani is attached to the malleus (one of the three ossicles in the middle ear cavity). It is innervated by the Vth Cranial or Trigeminal Nerve and contraction of the tensor tympani draws the malleus medially and anteriorly. The stapedius muscle attaches to the neck of the stapes (another of the ossicles), is innervated by the VII or Facial Nerve and upon contraction, draws the stapes outward and backward from the oval window, counteracting the opposite pull of the tensor tympani. These muscles have two opposing functions: first, to increase the sensitivity of the tympanic membrane and the ossicular chain to sounds of weak intensity, and second, to protect the inner ear from sounds of unusually loud intensity by reducing the mobility of the ossicular chain, thus decreasing the efficiency of sound transmission (Zemlin, 1968; Lamb and Norris, 1969; Davis and Silverman, 1970; Newby, 1972) although this latter function is now in question (Jerger, 1974).

The contraction of the muscles of the middle ear in response to loud sound, termed "acoustic reflex," usually is elicited at sound intensities well above the threshold for hearing. In man, it is elicited at intensities ranging from 80 - 90 dB above the pure-tone threshold for hearing, with the lowest reflex threshold corresponding in frequency to the lowest threshold for hearing (Jepsen, 1963). Luscher (cited by Jepsen, 1963) used tones throughout the frequency
range of 90 to 14,000 Hz to demonstrate reflex activity and found that the most sensitive frequency for eliciting the reflex was 2,000 Hz.

The muscle contraction is set off by a reflex action from the lower centers of the brain a few hundredths of a second after the sound reaches the eardrum. This reflex results in a modicum of protection against possible damage by large amplitudes of movement to the middle ear and the inner ear. Moreover, there is a latency between the time that the sound impinges upon the tympanic membrane and the contraction of the muscles. Wever and Lawrence (1954) cite mean latency values of .06 seconds for the stapedius and .15 seconds for the tensor tympani. This factor places a real limitation upon the "protection" that the tympanic muscles can provide to the middle and inner ears.

More recent studies have indicated that it is probably the stapedius muscle alone that responds to sound with a recordable reflex; therefore, many authors prefer to use the term "stapedius reflex" in conjunction with middle ear reflex action (Klockhoff, 1961; Jepsen, 1963; Feldman, 1967; Jerger, 1974). Most authors agree that the most efficient way of measuring reflex activity in man is through the use of relative impedance methods.

Sound Transmission in the Ear

Before describing the principles of impedance measurements, it may be beneficial to consider the propagation of sound in the normal ear. When an acoustic wave reaches the tympanic membrane, the greater part of its energy is reflected and a portion produces a vibration of the eardrum. This latter part is transmitted via the ossicular chain through the oval window to the inner ear. The reflected energy forms
a wave that is propagated outward from the tympanic membrane. Its frequency is identical to that of the incident wave. However, its phase and amplitude are dependent upon the impedance at the eardrum, which in turn, is controlled by the properties of the membrane, ossicular chain, ligaments and muscles of the middle ear, the oval and round windows, the middle ear cavity, and the interconnected pneumatic cells. Therefore, the sound wave reflected at the tympanic membrane carries information concerning the state of the entire middle ear (Zwislocki, 1961).

Clinical Methods of Measuring Acoustic Impedance

The concept of acoustic impedance was introduced by A.G. Webster in 1914, but was not widely utilized until Metz (1946) adapted these principles for use in the development and construction of the acoustic bridge. He was able to demonstrate that various pathological middle ear conditions produce different and distinct patterns of impedance. The Metz Bridge, however, was unwieldy, difficult to use, and did not yield stable measurements. Furthermore, the bridge could not control the effect of the volume of the ear canal on the measurement. It was not until the reports of Zwislocki (1963) and Feldman (1963) that the use of the acoustic bridge for measuring impedance provided meaningful information for the differential diagnosis of auditory disorders.

The Zwislocki Acoustic Bridge, shown schematically in Figure 1, is based upon the same principles as those described by Metz. However, this instrument included a means by which the effects of the volume of the ear canal could be eliminated from the measurement. This was accomplished by filling the ear canal with alcohol from a calibrated
syringe. Volume $V_1$ on the instrument is set to the measured volume of the canal as shown on the syringe.

![Figure 1. Schematic illustration of the Zwislocki Acoustic Bridge (Lamb and Norris, 1969).]

The Bridge consists of two main tubes (A and B) of equal internal diameter and length with an electro-acoustic transducer (T) mounted between them. The monitor tube (Y) leads to the examiner's ears. Tube A is connected to the ear canal via a speculum; tube B terminates in the matching impedance. The transducer (T) presents sound waves of equal amplitude, but opposite phase into the two main tubes. These waves are partially reflected at the ends of each tube and the resultant sound pressure in each tube is generated by both the original and the reflected waves. The sound pressure in both tubes is equal when both are terminated by an equal impedance. A null or cancellation of sound occurs as a result of the phase opposition, and can be detected by monitoring the Y tube. When this occurs, the impedance at the end of the tube (B) is equal to the unknown impedance of the tympanic membrane and the middle ear, and may be read directly from the variable controls, $V_2$ (compliance element) and $R_A$ (resistance element).

Two additional tests may be performed: tactile stimulation around the tragus of the test ear, or introduction of noise or tone to the contralateral ear. The presence of the stapedius reflex will re-
result in a return to the probe tone (a loss of the null or sound cancellation) as monitored by the examiner. The null returns when either mode of stimulation ceases (Feldman, 1963).

Both the Metz and the Zwislocki Bridges used ambient air pressure to measure acoustic impedance. In 1960, Terkildsen and Neilsen developed an electroacoustic bridge which provided a source of air pressure that was continuously variable from a negative value, through zero, to a positive value. The two electroacoustic bridges developed for clinical use are the American Electroacoustic Impedance Meter (formerly, the Madsen Acoustic Impedance Meter) and the Grason-Stadler Otoadmittance Meter, using the balancing system originally introduced by Terkildsen and Neilsen (1960). Nearly all of the research data available at this time concerns the use of the Madsen Acoustic Impedance Meter, notably the work of Brooks (1968, 1969, 1971), Jerger (1970), and Lilly (1973).

**Impedance Measurements**

The measurement under consideration is the extent to which the tympanic membrane is resistant to movement and opposes the sound pressure changes. This opposition to change, or resistance to motion, represents the acoustic impedance of the ear. In other words, acoustic impedance may be defined as the opposition by a surface to the flow of acoustic energy through that surface. Three components may interfere with or impede the flow of acoustic energy: stiffness, mass, and resistance. Stiffness in the middle ear is produced by the tympanic membrane, the ligaments and muscles of the middle ear, the volume of air in the middle ear, and the cochlear windows. Mass is determined by the weight of the ossicular chain; the resistance is determined by the in-
put impedance of the cochlea and to some extent, by the frictional resistance of the ossicles (Zwislocki, 1963).

When the middle ear system is unusually stiff, as in the presence of otosclerosis, the tympanic membrane presents a greater than normal resistance to motion; that is, it is less compliant. Little sound energy is transmitted through the middle ear system, and a greater than normal amount is reflected from the membrane. This condition is said to have a high impedance factor. In an ear with ossicular discontinuity, the membrane is extremely compliant, with a large amount of energy absorbed by the membrane and little reflected back into the external auditory meatus. This condition shows extremely low acoustic impedance (Feldman, 1963).

Tympanometry

The concept of tympanometry may be defined as a technique for measuring, recording, and evaluating changes in acoustic impedance with systematic changes in air pressure. The relationship between changes in acoustic impedance and changes in air pressure is affected by middle ear pathologies, perforations of the tympanic membrane or scars of the membrane, or by abnormal air pressures in the middle ear. For example, if fluid is present in the middle ear, the point of maximum compliance will be displaced and the degree of compliance reduced. Figure 2 compares a normal and a pathological tympanometric curve.

Conditions such as otosclerosis and ossicular chain discontinuity appear as changes in the compliance of the tympanic membrane, but show no pressure anomalies. Otosclerosis causes the conductive system to be stiff or non-compliant, while an interruption in the ossicular chain or
a scarred tympanic membrane results in abnormally high compliance. Negative air pressure in the middle ear cavity produces a curve displaying a shift to the left of 0 mm H₂O, and a shift of 100 mm H₂O or more is associated with Eustachian tube malfunction. An ear which

contains fluid also displays a negative curve configuration. Because of the stiffening influence of the fluid, the tympanic membrane will not achieve normal compliance and thus can be differentiated from the other curves (Lamb and Norris, 1969).

**Reflex Measurements**

In a normal middle ear, contraction of the stapedius or the tensor tympani muscle produces a "measurable, time-locked change in acoustic impedance at the lateral surface of the tympanic membrane" (Lilly, 1973). With the use of electroacoustic instrumentation, reflex measurements are termed relative acoustic impedance measurements. The threshold of the acoustic reflex is that sensation level at which a
sound is just capable of eliciting a reflex contraction. The reflex threshold falls within a predictable range of intensities, adding to the diagnostic usefulness of impedance measurements (Lamb and Norris, 1969).

Jepsen (1963) reported studies of the acoustic reflex to pure tones in normal subjects ranging in age from ten to eighty years. He found that while the auditory thresholds were poorer in the older subjects as compared to the younger group, there was an increase in the sensitivity of the acoustic reflex thresholds. This change occurred at each frequency, but was more pronounced above 1000 Hz. For example, at 4000 Hz, the range between thresholds was reduced to 15 dB for the eighty year old subjects. This reduced range is assumed to be a manifestation of loudness recruitment, resulting from cochlear dysfunction.

Although the absence of the stapedius reflex usually indicates middle ear pathology, the reflex cannot always be elicited. There appears to be a very small percentage of otherwise normal individuals who do not show the acoustic reflex at any level. When the reflex is elicited acoustically, the success depends upon a sufficiently low hearing level. The absence of the reflex does not always indicate the presence of a middle ear disorder, nor does a detectable reflex contraindicate the presence of pathology. The reflex has been found in some sites of ossicular discontinuity and serous otitis media. Thus, although relative impedance does not always give a true diagnostic picture, when used in combination with tympanometry, a correct diagnosis can be made (Robertson et al., 1968; Jerger, 1970; Zwislocki, 1970).

**Normative Standards**

Feldman (1974) established normative tympanometric curves with
the Grason-Stadler Otoadmittance Meter on 100 normal adult subjects. These subjects had no otologically confirmed middle ear involvement and were either audiometrically normal or manifested only sensori-neural impairment. Dirks and Morgan (1973) established normative data on 52 subjects. Porter (1972) established normative otoadmittance values for 10 normal hearing adults. Jacobson, et al., (1973) developed normative standards for clinical use of the Otoadmittance Meter by conducting tympanometry on 30 normal young adults. The data gathered by these researchers are displayed on Tables II and III (pages 26 and 27).

Diagnostic Implications

Tympanometry has become, in many clinics, an invaluable diagnostic tool and a routine part of the audiological assessment of every patient. The procedure is reasonably simple and rapid and has been used successfully with persons of all ages. Jerger (1970) reports on the use of tympanometry with infants, and Brooks (1968, 1971) has used this method successfully on school age children. Because standard procedures using pure-tone air- and bone-conduction audiometry are often difficult to administer, tympanometry has been found to be of value with mentally retarded patients because only passive cooperation is required of the subject (Lamb and Norris, 1969). In addition, there appears to be a higher than normal incidence of conductive disorders among the mentally retarded, therefore, tympanometric measurements may be particularly useful.

Although tympanometric methods in clinical practice have been in use for slightly more than a decade, little information has been found on their use with the elderly. A possible reason for this might be
that because tympanometry is used to evaluate middle ear pathologies and hearing loss in the elderly is primarily a sensori-neural impairment, there appeared to be little reason to employ this instrumentation. Hinchcliffe (1962), in a personal communication with A. Møller, quotes Møller as stating that changes in the acoustic impedance of the middle ear as a function of age have not been noted. Tympanometry was used on 316 patients of all ages by Jerger (1970). Of this number, fifty-five subjects were sixty years of age or over, or seventeen percent of the total population. However, none had normal hearing sensitivity and a conductive or sensorineural component was present in all of these subjects.

Changes in Hearing Associated with Aging

It is well known that there is a change in hearing level with age and this gradual reduction in hearing sensitivity associated with increased age has been termed "presbycusis." In most cases, both ears are affected at about the same rate and the loss occurs gradually over the years.

In the earliest stages of presbycusis, only the epithelial elements in the cochlea may be affected. At this point, the impairment is classified as sensory in origin. Later, the nerve elements become involved and the classification is thought to be sensori-neural. Finally, the cortex and the central pathways become involved and the condition is classified as a central hearing impairment, or central dysacusis. In other cases, the nerve fibers appear to be damaged and the impairment is considered to be primarily a neural hearing impairment (Sataloff, 1966).
Although presbycusis is generally considered to be a sensorineural impairment, Glorig and Davis (1961) identified a conductive element, whose presence was indicated by an air-bone gap. They labeled this type "conductive presbycusis." In their sample of elderly who had no noise exposure that could be judged as severe by modern standards, the shift in threshold sensitivity due to presbycusis had an appreciable conductive element. The precise contribution that this high tone conductive loss makes to presbycusis in the general population is not yet clear.

Goodhill (1969) used the same term (conductive presbycusis) to identify the changes found in the middle ear as a result of aging. He stated that the term "presbycusis" should not be limited to losses of a sensorineural nature. If aging processes occur in the ligaments and muscles and connective tissue, then it is possible and quite likely that changes due to senescence may occur in the middle ear involving the ossicular chain and the tympanic membrane. These changes, which may be normal or premature, may cause a variety of aging lesions which are not sensorineural, but conductive in nature.

According to Hinchcliffe (1962), thresholds in the elderly show a departure from the basic presbycusis trend and portray a hearing loss greater than the predicted loss. The discrepancy between predicted and actual thresholds is greater with tones of higher frequency and with increasing age. It is possible, then, that "the high frequency conductive loss could account for this discrepancy and constitute a major secondary factor in the deterioration of the auditory threshold with age" (Hinchcliffe, 1962).

Goetzinger, et al. (1961) established curves of average hearing
levels for men and women from ages 60 to 90 inclusive. The criteria for selection of a subject included no history of hearing loss prior to age fifty, he must have been relatively free from ear infections during life, and have had relatively little exposure to noise. They found that hearing level decreases as a function of increasing age, that men have more acute hearing in the lower frequencies and women in the higher frequencies, and that the hearing level for both men and women drops off markedly for the higher frequencies with increased age. Table I shows the means, standard deviations, and ranges for the pure tone air-conduction thresholds by age and by sex.

**TABLE I**

RANGES OF HEARING LEVELS BY AGE GROUPS AND SEX OF SELECTED OLDER ADULTS. THESE HEARING LEVELS IN dB re ISO-1964 AUDIOMETRIC ZERO WERE COMPUTED FROM SOUND PRESSURE LEVELS PRESENTED BY GOETZINGER, ET AL. (1961)

Frequencies in Hz

<table>
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<tr>
<th>Age</th>
<th>Sex</th>
<th>250</th>
<th>500</th>
<th>1000</th>
<th>2000</th>
<th>4000</th>
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<tr>
<td>60-69</td>
<td>M</td>
<td>-10 to 20</td>
<td>-10 to 26</td>
<td>-10 to 30</td>
<td>-10 to 51.5</td>
<td>4 to 64</td>
</tr>
<tr>
<td></td>
<td>F</td>
<td>-10 to 10</td>
<td>-10 to 11</td>
<td>-10 to 15</td>
<td>-8 to 31.5</td>
<td>-4 to 59</td>
</tr>
<tr>
<td>70-79</td>
<td>M</td>
<td>-10 to 5</td>
<td>-10 to 21</td>
<td>-10 to 30</td>
<td>-10 to 56.5</td>
<td>19 to 69</td>
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<tr>
<td></td>
<td>F</td>
<td>-10 to 15</td>
<td>-10 to 16</td>
<td>-10 to 35</td>
<td>-3 to 46.5</td>
<td>9 to 64</td>
</tr>
<tr>
<td>80-89</td>
<td>M</td>
<td>-10 to 25</td>
<td>-4 to 31</td>
<td>0 to 35</td>
<td>6.5 to 56.5</td>
<td>44 to 89</td>
</tr>
<tr>
<td></td>
<td>F</td>
<td>-5 to 30</td>
<td>-9 to 26</td>
<td>0 to 30</td>
<td>-3 to 36.5</td>
<td>14 to 94</td>
</tr>
</tbody>
</table>

Hinchcliffe (1962) reported on studies by Fleischer and by Crowe, et al., who state that presbycusis is predominantly a "ganglion type" deafness. In other words, atrophy of the spiral ganglion cells occurs
in later years. Hinchcliffe observed that threshold shifts due to aging begin at an early age and atrophy of the spiral ganglion cells appear much later in life. In many cases, elderly people have had considerable threshold shifts due to aging, but have shown no histological changes in either the organ of Corti or in the spiral ganglion.

Goetzinger, et al. (1961) studied men and women between the ages of eighty and one hundred who showed no significant tone decay. They concluded that the degenerative changes in the cochlea and in the second-, third-, and fourth-order neurons are not dominant factors in the development of presbycusis.

The conclusions drawn from Hinchcliffe's exhaustive review of the literature regarding changes in the aging auditory system indicate that although degenerative changes contribute to presbycusis, it is more likely that changes in the brain are primarily responsible for the overall effect of presbycusis. "The relative contribution of the degenerative changes in different anatomical loci to changes in a given audiologic measure is variable and dependent upon the particular measure involved" (Hinchcliffe, 1962).
CHAPTER III

METHOD

In order to gather data which may be used toward establishing working norms on tympanometric curves obtained from an elderly population, the following methods and procedures were utilized.

Subjects

Forty subjects who, upon screening, were classified as "normal older adults" were chosen to participate in this study. The majority of the subjects were selected from among those individuals who had been screened by Project ARM (Auditory Rehabilitation Mobile), sponsored by Portland State University. The following criteria were employed to select subjects suitable for this study: 1) over fifty-nine years of age; 2) auditory acuity commensurate with his age (Goetzinger et al., 1961); 3) negative history of middle ear pathology; 4) normal tympanic membranes as determined by otologic examination.

The ages of the forty subjects ranged between fifty-nine and eighty-three years of age, mean age = 69.8. Only those tympanograms in which maximum values fell within ± 50 mm H2O of ambient pressure were included. Tympanometry was performed on both ears of each subject; however, if one ear presented an abnormal tracing, only the other "normal" ear of the subject was included in this study.

Instrumentation

The Grason-Stadler Otoadmittance Meter (Model 1720) consists of
Figure 3. Schematic representation of the Grason-Stadler Otoadmittance Meter, Model 1720 (Porter, 1972).
three subassemblies (see Figure 3): one for the control of air pressure, one for the generation and monitoring of sound waves, and one for the electronic control and evaluation of the input sound flow and the output sound pressure conditions.

The air pressure system presents a continuously variable positive or negative air pressure to the ear canal and this feature permits the stiffening of the tympanic membrane in order to estimate the conductance and susceptance of the ear canal. The transducer or driver/monitor assembly, consisting of an earphone driver and ceramic microphone, is mounted in a housing connected to the earpiece. Sound energy is introduced into the ear canal, modified by the conditions it encounters in the canal and at the tympanic membrane, and is picked up by the microphone. The analysis system maintains a constant sound pressure level of approximately 85 dB SPL at the tympanic membrane, regardless of conditions found there.

The sound flow required to maintain constant pressure in the ear canal is 90° out-of-phase with the pressure, if the ear is free of energy loss. Energy losses result in an in-phase component. The in- and out-of-phase components are measured separately and may be read directly on the two meters as susceptance and conductance, expressed in millimhos (Otoadmittance Handbook 2, 1973).

The voltages representing conductance and susceptance are available to drive an X-Y plotter from the rear of the instrument, as well as a voltage which is proportional to the air pressure in the ear canal. A graphic record can then be made depicting the relationship between compliance changes as a function of variation of pressure in the ear canal (Porter, 1972). Thus a tympanogram is generated whose charac-
teristic pattern is diagnostically invaluable.

**Measurement**

The unit of measurement under consideration is admittance, or ease of energy flow, which is the reciprocal of impedance. The components of impedance, resistance and reactance, are termed conductance ($G_A$) and susceptance ($B_A$) respectively. Conductance is a measure of energy flow through resistance while susceptance is a measure of energy flow through reactance. Susceptance can be equated to compliance, commonly thought of as the reciprocal of stiffness. Using admittance terminology, the unit of admittance is the mho (ohm spelled backward) (*Otoadmittance Handbook 2, 1973*).

When the tympanic membrane is stiffened by the introduction of air pressure, the admittance at the drum is approximately zero and the value of admittance is that of the ear canal. When the air pressure is equal on both sides of the drum, the admittance measured is the sum of the admittance of the ear canal and the admittance of the drum. Admittance is said to be the ratio of sound flow to sound pressure and is constant within the ear canal when a low probe tone frequency is used. Sound flow, and therefore admittance, for the tympanic membrane is the difference between the drum tight and the drum loose measurements (*Porter, 1972*).

Admittance can be calculated according to the following method:

$$|Y| = \sqrt{G^2 + B^2}$$

where $Y$ = admittance, $G$ = conductance, $B$ = susceptance. Since admittance is the reciprocal of impedance ($Z$), the latter may be determined by the formula:

$$|Z| = \frac{1}{Y}$$ (*Otoadmittance Handbook 2, 1973*).
**Test Procedure**

Immediately prior to this evaluation, each individual was subjected to an otoscopic examination. When a large amount of cerumen, which precluded viewing the tympanic membrane, was present, the ear was washed out before the examination proceeded.

Pure tone air- and bone-conduction testing were done in a single-wall IAC Model SP 403 room using a Beltone 15-C audiometer. Norms for air conduction audiometry were those established by Goetzinger et al. (1961) for individuals of advanced age. His data, based on ASA-1951 standards were converted to ISO-1964 standards (see TABLE I on page 15). Speech audiometry consisted of obtaining the following measures: speech reception threshold, most comfortable listening level (MCL), and speech discrimination ability. The latter was determined by a live voice presentation of the Campbell Word List.

The otoadmittance meter was checked for calibration at the beginning of each test day. Tympanometry was administered using the Grason-Stadler Model 1720, and the admittance values were plotted by means of a Hewlett-Packard, Model 7035B X-Y recorder. The values for conductance and susceptance were plotted for each of the two test frequencies, 220 and 660 Hz, under conditions of decreasing ear canal pressure (from +200 to -200 mm H₂O).

The otoadmittance meter was used in the IAC room, although a sound-treated room is not necessary for the administration of tympanometry. The subject was seated in a chair facing the instrument, and the examiner explained the procedure to him as the test progressed. The subject was told to refrain from talking or moving, and to avoid any unnecessary swallowing, yawning, clearing of throat, or coughing.
The subject was allowed to view the meters on the instrument. This reduced extraneous movements since he was able to note the needle movement caused by moving or swallowing.

After obtaining an airtight seal in the subject's ear, the first recording of susceptance was made at 220 Hz, from conditions of positive to negative pressure, and then at 660 Hz. The same procedure was used to record conductance at 220 Hz and 660 Hz. The pressure was returned to the maximum value of admittance and the reflex thresholds were noted. The procedure was as follows: pure tones were presented via earphone to the ear opposite the probe tip. The otoadmittance meter was set to the AGB position which centers both meters and increases the sensitivity of the instrument. Tone presentation was administered in ascending 5 dB steps and the acoustic reflex threshold was determined if either meter showed a ten percent deflection of the needle to the left.

Fifty ears of the eighty tested proved to be "normal" and were used in this investigation; sixteen ears or twenty percent of the sample produced tympanograms suggestive of a healed perforation. According to Jerger (1974), at least fifteen percent of "normals" display this "w" shaped tympanometric configuration. Nine ears in this sample produced configurations that were shallow or flat, or a tracing which was not within 50 mm H2O of ambient air pressure; and a seal could not be obtained on five ears. From this sample of forty older adults, both ears of nineteen subjects were normal and were included in this study; twelve subjects had only one normal ear that could be utilized.

Retesting

Tympanometry was re-administered as a check of reliability within
a two-week period to six of the subjects and a total of ten ears was utilized from this sample. One of the subjects reported a problem which was indicative of conductive pathology at one ear. Administration of tympanometry revealed the presence of conductive pathology, later confirmed by otoscopic examination. One ear of another subject proved impossible to seal during the retest session.
Results

The ranges for conductance and susceptance obtained from an older adult population are displayed in Figure 4 in template form. The upper and lower tracings at 0 mm H₂O pressure represent the 90th and 10th percentile points. TABLE II presents these same data plus the ranges and medians for admittance (Yₐ) and impedance (Zₐ). For comparative purposes, the figures obtained from one hundred normal ears (Feldman, 1974) are included on the table.

TABLE III includes group data for conductance, susceptance, admittance and impedance obtained from the older adult group. Included on the table are results reported by other researchers and obtained by them from “normal, young adult groups.”

Means and standard deviations for reflex thresholds are shown in TABLE IV. Reflex thresholds were obtained at 500, 1000 and 2000 Hz and the data were averaged because there was no significant difference related to the stimulus frequency. Reflex thresholds were slightly better at the higher probe tone (660 Hz), but the difference between the 220 and 660 Hz probe tones was not significant. Similar data from Porter (1972) are displayed. He pointed out that the thresholds obtained using the 660 Hz probe were more acute than those from the 220 Hz probe, but that the largest difference was less than the usual 5 dB step utilized in clinical determination of thresholds.
Figure 4. Ranges of 50 normal ears obtained from an older adult population. The upper and lower boundaries at 0 mm H$_2$O and 200 mm H$_2$O pressure are the 90th and 10th percentile respectively.
TABLE II

SUSCEPTANCE, CONDUCTANCE, ADMITTANCE IN MMHOS
AND IMPEDANCE IN OHMS:
MEDIANs AND RANGES

<table>
<thead>
<tr>
<th></th>
<th>220 Hz</th>
<th>660 Hz</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>B&lt;sub&gt;A&lt;/sub&gt;</td>
<td>G&lt;sub&gt;A&lt;/sub&gt;</td>
</tr>
<tr>
<td>50 Normal Ears (Fine)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>80% Range</td>
<td>.3-.65</td>
<td>.15-.5</td>
</tr>
<tr>
<td>Medians</td>
<td>.5</td>
<td>.3</td>
</tr>
<tr>
<td>100 Normal Ears (Feldman, 1974)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>80% Range</td>
<td>.3-.75</td>
<td>.05-.35</td>
</tr>
<tr>
<td>Medians</td>
<td>.5</td>
<td>.15</td>
</tr>
</tbody>
</table>
# TABLE III

GROUP DATA FOR CONDUCTANCE, SUSCEPTANCE, ADMITTANCE IN MILLIMHOS, AND FOR IMPEDANCE IN OHMS

<table>
<thead>
<tr>
<th></th>
<th></th>
<th></th>
<th></th>
<th></th>
<th></th>
<th></th>
<th></th>
<th></th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>$G_A$</td>
<td>$B_A$</td>
<td>$Y_A$</td>
<td>$Z_A$</td>
<td>$G_A$</td>
<td>$B_A$</td>
<td>$Y_A$</td>
<td>$Z_A$</td>
</tr>
<tr>
<td>Older Adults (Fine)</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>$\bar{x}$</td>
<td>.32</td>
<td>.49</td>
<td>.59</td>
<td>1895</td>
<td>2.47</td>
<td>1.12</td>
<td>2.72</td>
</tr>
<tr>
<td>n = 50 ears</td>
<td>s.d.</td>
<td>.16</td>
<td>.16</td>
<td>.21</td>
<td>690</td>
<td>1.00</td>
<td>.53</td>
<td>1.04</td>
</tr>
<tr>
<td>59-83 years</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Young Adults (Porter, 1972)</td>
<td>$\bar{x}$</td>
<td>.35</td>
<td>.71</td>
<td>.79</td>
<td>1265</td>
<td>2.75</td>
<td>1.01</td>
<td>2.93</td>
</tr>
<tr>
<td>n = 36 ears</td>
<td>s.d.</td>
<td>.08</td>
<td>.22</td>
<td>-</td>
<td>-</td>
<td>1.01</td>
<td>.48</td>
<td>-</td>
</tr>
<tr>
<td>18-40 years</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Young Adults (Dirks &amp; Morgan, 1973)</td>
<td>$\bar{x}$</td>
<td>.26</td>
<td>.65</td>
<td>.71</td>
<td>1616.1</td>
<td>1.91</td>
<td>1.29</td>
<td>2.34</td>
</tr>
<tr>
<td>n = 104 ears</td>
<td>s.d.</td>
<td>.13</td>
<td>.23</td>
<td>.28</td>
<td>574.9</td>
<td>1.09</td>
<td>.54</td>
<td>1.16</td>
</tr>
<tr>
<td>Young Adults (Jacobson et al., 1973)</td>
<td>$\bar{x}$</td>
<td>.28</td>
<td>.58</td>
<td>-</td>
<td>-</td>
<td>1.7</td>
<td>.83</td>
<td>-</td>
</tr>
<tr>
<td>n = 60 ears</td>
<td>s.d.</td>
<td>.24</td>
<td>.23</td>
<td>-</td>
<td>-</td>
<td>1.0</td>
<td>.50</td>
<td>-</td>
</tr>
<tr>
<td>18-30 years</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

27
<table>
<thead>
<tr>
<th>Probe tone</th>
<th>Older Adults Fine</th>
<th>n=23</th>
<th>Adults Porter (1972)</th>
<th>n=18</th>
</tr>
</thead>
<tbody>
<tr>
<td>220 Hz</td>
<td>94.2</td>
<td>9.20</td>
<td>88.2</td>
<td>5.78</td>
</tr>
<tr>
<td>660 Hz</td>
<td>92.9</td>
<td>9.15</td>
<td>85.9</td>
<td>6.20</td>
</tr>
</tbody>
</table>
Six of the forty subjects were retested within a two-week period using the same procedures as originally employed. Two of the subjects' ears were not included in this correlation: one appeared to have a mild middle ear infection in one ear resulting in a negative excursion in the tracing for that ear; the other subject had one ear upon which a seal could not be obtained. Therefore, from the six subjects, a total of ten ears were used. The means and standard deviations for these ten normal ears are shown on TABLE V. The results of the Pearson Product-Moment Correlation between the first and second test procedure revealed a high correlation and were significant at the levels shown.

Discussion

The ranges for $B_A$ and $G_A$ obtained from a normal older adult population are shown schematically on Figure 4. The upper and lower boundaries of each measurement represent the 90th and 10th percentile points at ambient atmospheric pressure. Measurements obtained from otologically normal older adults will fall within the limits displayed. The configurations do not necessarily portray the actual shape of the tympanogram obtained from changing air pressure in the ear canal.

The ranges and medians for $B_A$, $G_A$, $Y_A$, and $Z_A$ are reported on TABLE II, as well as those reported by Feldman (1974) for one hundred normal ears obtained from a younger sample. The median value of susceptance ($B_A$) at 220 Hz is $0.5$ mmho and agrees with Feldman's value of $0.5$ obtained on one hundred normal young ears. The median values for the other measurements are in good agreement as well. Feldman stated that prior to his study, there were no reports of similar measurements with the otoadmittance meter. However, on TABLE III are gathered group
<table>
<thead>
<tr>
<th>Probe tone frequency</th>
<th>Initial test</th>
<th>Retest</th>
<th>Initial Test</th>
<th>Retest</th>
<th>r</th>
<th>&lt;</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>x</td>
<td>x</td>
<td>s.d.</td>
<td>s.d.</td>
<td></td>
<td></td>
</tr>
<tr>
<td>B 220 Hz</td>
<td>.49</td>
<td>.43</td>
<td>.13</td>
<td>.17</td>
<td>.765</td>
<td>&lt; .01</td>
</tr>
<tr>
<td>G 220 Hz</td>
<td>.29</td>
<td>.29</td>
<td>.13</td>
<td>.09</td>
<td>.905</td>
<td>&lt; .001</td>
</tr>
<tr>
<td>Y 220 Hz</td>
<td>.57</td>
<td>.52</td>
<td>.16</td>
<td>.19</td>
<td>.874</td>
<td>&lt; .001</td>
</tr>
<tr>
<td>Z 220 Hz</td>
<td>1886.5</td>
<td>2192.1</td>
<td>602.9</td>
<td>787.8</td>
<td>.799</td>
<td>&lt; .01</td>
</tr>
<tr>
<td>B 660 Hz</td>
<td>1.19</td>
<td>1.06</td>
<td>.57</td>
<td>.51</td>
<td>.97</td>
<td>&lt; .001</td>
</tr>
<tr>
<td>G 660 Hz</td>
<td>2.57</td>
<td>2.27</td>
<td>.89</td>
<td>.77</td>
<td>.85</td>
<td>&lt; .01</td>
</tr>
<tr>
<td>Y 660 Hz</td>
<td>2.69</td>
<td>2.55</td>
<td>.97</td>
<td>.74</td>
<td>.90</td>
<td>&lt; .001</td>
</tr>
<tr>
<td>Z 660 Hz</td>
<td>428.8</td>
<td>420.0</td>
<td>93.0</td>
<td>108.5</td>
<td>.73</td>
<td>&lt; .02</td>
</tr>
</tbody>
</table>

Critical Values for r: .001 = .872
 .01 = .765
 .02 = .716
data for these measurements as reported by Porter (1972), Dirks and Morgan (1973), Jacobson et al. (1973), as well as the older group investigated in this study. The latter three researchers utilized what they termed "normal young adult" populations. Upon surveying their results, it can be seen that there is a wide variance among the three studies, particularly those obtained with the 660 Hz probe tone.

Porter (1972) found that the reflex thresholds obtained from his young normal group were slightly more acute using the 660 Hz probe tone. This was true with the older group as well, but not at a significant level. Some researchers believe that the higher frequency probe tones (660 or 800 Hz) are preferable to 220 Hz because the change in impedance which occurs with the reflex muscle contraction is greater near the resonant frequency of the middle ear (Möller, 1960; Linden et al., 1972). However, Jerger (1974) found that by manipulating the probe tone frequency, there is a point at which the reflex disappears. In most normals, this occurs between 600 and 700 Hz. Therefore, when investigating abnormalities in the acoustic reflex, the least desirable frequency range to use would be between 600 and 700 Hz.

Clinical Observations

The results of this investigation on the aging are consistent with tympanometric values obtained by other investigators on normal young adults. This suggests that the otoadmittance meter is a valuable adjunct in the routine examination of older adults as well as in younger populations where it has already been established as a necessary part of the audiologic examination. In addition to the forty subjects selected to participate in this study, the otoadmittance meter has been
used routinely in the assessment of older adults referred to Portland State University's Project ARM (Auditory Rehabilitation Mobile), a service designed to aid the low-income hard-of-hearing elderly.

The otoadmittance meter is relatively simple to operate and the complete recording of the tympanogram and the acoustic reflex thresholds for both ears can be completed in approximately twenty minutes. The procedure is not uncomfortable to the subject and an adequate seal can be quickly obtained in nearly all cases. Among the subjects used in this investigation, a seal could not be obtained in one female in one ear and in two male subjects in both ears. One of the latter subjects voluntarily returned to the clinic on three occasions, but a seal was not secured because of his abnormally large ear canals. In most cases, an adequate seal is obtained on the first attempt.

One of the interesting aspects of this investigation related to the number of ears that were found, upon inspection, to be otologically normal, but whose tympanograms indicated the presence of a healed perforation. From the eighty ears included in this survey, sixteen produced configurations suggestive of a scarred tympanic membrane. The subjects claimed no memory of middle ear infection and scarring was not noted during otoscopic examination.

Ears having a healed perforation usually yield distinctive tympanograms. At 660 Hz, the conductance \((G_A)\) curve will exhibit a large amplitude with a single peak and the susceptance curve \((B_A)\) will display a notch which may coincide with the conductance peak. Figure 5 is a schematic drawing of this type of tympanogram. In some cases, all four tracings will display sharp peaks. The greater amplitude of the configuration precludes measurement of conductance and susceptance.
Figure 5. Tympanogram resulting from a healed perforation (Otoadmittance Handbook 2, 1973).
(static impedance), and invalidates the use of tympanometry in the differential diagnosis of middle ear pathologies.

Research Implications

Although the present investigation provides data on a small number of subjects, a larger sample should be utilized in order to establish additional normative data on an otologically normal older adult population. Research may be directed, not only toward between-subject, but between-ear measurements on this age group. Additionally, the reflex thresholds should be measured across the entire frequency range on normal young and normal older adult groups, and an analysis of variance made. These additional data would make possible the utilization of the otoadmittance meter for clinical use with aged subjects.
CHAPTER V

SUMMARY AND CONCLUSIONS

Investigations utilizing electroacoustic measuring instruments designed to evaluate middle ear functioning have been made on children and on young adult populations. It appears, however, that there is no published research data available on tympanograms obtained from an elderly population. The results of the present study show that the use of tympanometry is valuable in the assessment of the status of the middle ear in the older adult as well as in younger populations. The purpose of the present study was to examine tympanometric configurations obtained from an otologically normal, older adult population. The information obtained may be used toward establishing working normative values using an otoadmittance meter.

The question under investigation was: What are the differences, if any, between tympanograms obtained from a normal young adult and those obtained from a normal older adult. Forty individuals were chosen to participate in this study. They ranged in age from 59 to 83 years of age and each had auditory acuity commensurate with his age. All of the subjects had a negative history of middle ear pathology and had normal tympanic membranes as determined by otologic examination. From the eighty ears tested, fifty were used in this survey.

Four measurements were obtained at each ear: conductance and susceptance at 220 Hz, and conductance and susceptance at 660 Hz. For each subject, the 220 Hz probe tone was utilized first. The measurement
under consideration was the amplitude of the curve obtained, and admittance was calculated from the conductance ($G_A$) and susceptance ($B_A$) components. Additionally, acoustic reflex thresholds were obtained from this population. The basis of these findings led to the following conclusions:

1) Tympanometry has been found to be a valuable adjunct in the assessment of the status of the middle ear in the older adult.

2) Results indicate that the values obtained for the measures of conductance and susceptance are comparable to those obtained from young adult groups.

3) The reflex thresholds are slightly higher (worse) in the older group than the younger group because their hearing thresholds are not as acute as those found in younger populations.

4) A larger percentage of the older population than might be expected was found to have evidence of healed perforations which were not found during otoscopic examination. These perforations affect the shape of the tympanometric configuration and may possibly obscure other pathologies.

The present investigation demonstrated that additional normative data are needed in order that the otoadmittance meter be fully utilized with older adult populations.
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Feldman, A., Impedance Measurements at the Eardrum as an Aid to Diagnosis. J. Speech and Hearing Research, 6, 315-327, 1963.


